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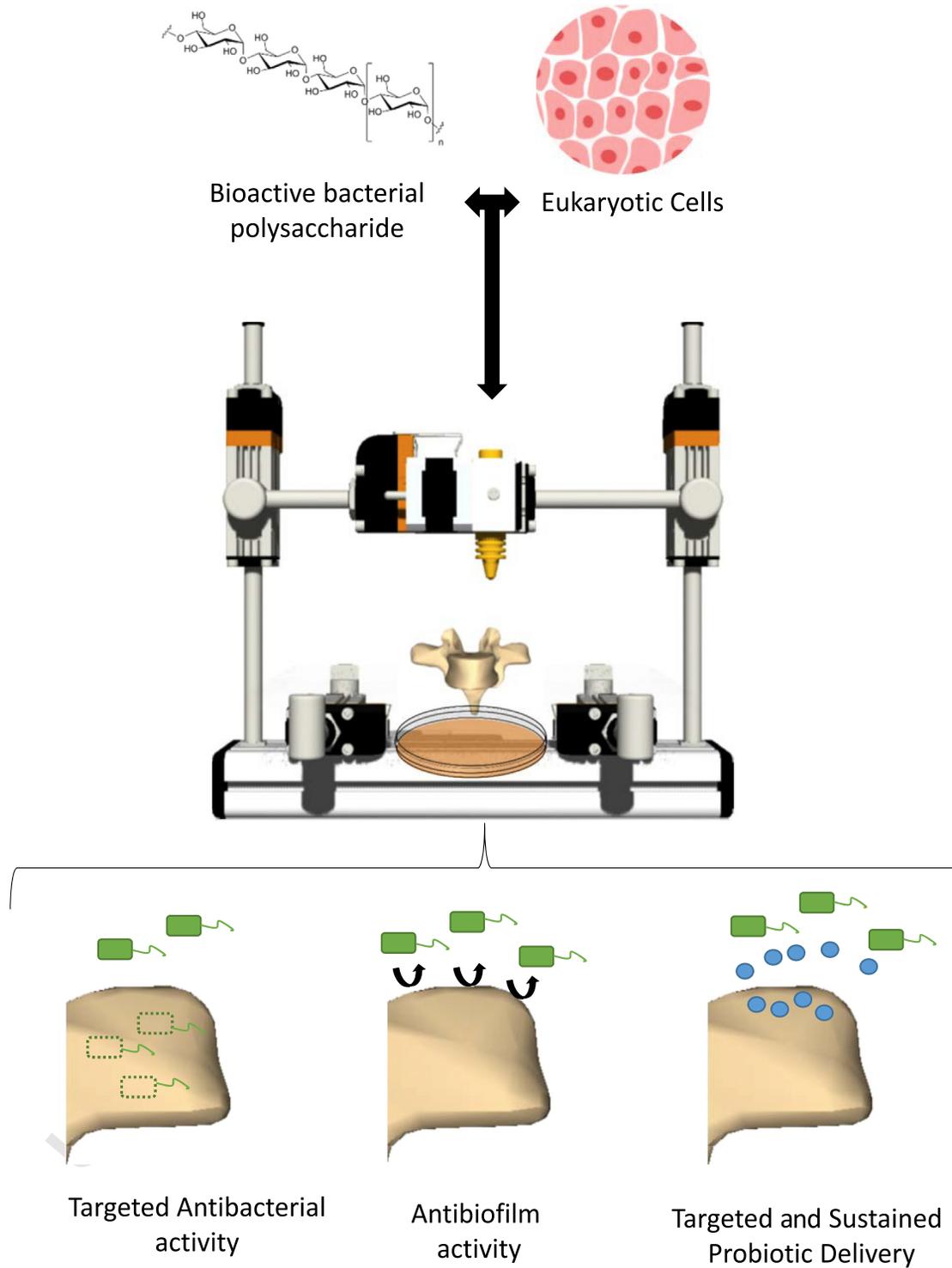
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Q2 Forum

3 Antimicrobial Inks:
4 The Anti-Infective
5 Applications of
6 Bioprinted Bacterial
7 PolysaccharidesQ4 Q3 Ronan R. McCarthy,^{1,*,@}
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10 Eujin Pei,³ and Guang Yang²
1112 **Bioprinting is a rapidly emerging**
13 **technology with the potential to**
14 **transform the biomedical sector.**
15 **Here, we discuss how a range**
16 **of bacterial polysaccharides with**
17 **antibiofilm and antibacterial activity**
18 **could be used to augment current**
19 **bioink formulations to improve**
20 **their biocompatibility and tackle**
21 **the spread of antibiotic-resistant**
22 **infections.**23 **Printing Bacteria and Bacterial**
24 **Polysaccharides**25 Additive manufacturing or 3D printing has
26 spearheaded a revolution in the biomedical
27 sector for rapidly prototyping medical
28 devices and personalized therapeutic
29 solutions. The field of 3D bioprinting
30 stemmed from the idea of combining 3D
31 printing, which uses layer-by-layer fabrication
32 techniques, with living organisms
33 and biomaterials to produce complex
34 tissues *in vitro*. Bioprinting can be classified
35 into four main process categories:
36 material jetting, laser-assisted printing,
37 stereolithography, and material extrusion.
38 Material jetting is a droplet-based technique
39 that provides a high-throughput
40 method with the ability to precisely control
41 the displacement of biological material. It
42 is compatible with a range of hydrogel
43 formulations, including alginate, agarose,
44 collagen, and fibrinogen [1]. Laser-
45 assisted printing uses laser-induced forward
46 transfer to pattern cells over a givensurface. This allows the positioning of
small volumes of cell suspensions with
high-resolution accuracy. This technology
has been used to print a range of cell
types, including embryonic stem cells,
with a limited impact on cell viability.
Stereolithography is a modified form of
laser-assisted printing that uses an energy
source, usually through laser curing or
ultraviolet (UV) light to selectively initiate
the polymerization process within a vat
containing the photosensitive polymer,
such as polyethylene glycol-diacrylate
(PEGDA) and gelatin methacryloyl [2].
Material extrusion is the most commonly
used method of bioprinting. It utilizes
physical forces, such as pneumatic pressure,
to force a bioink through an extrusion
nozzle and deposit it on a surface
substrate in a coordinated fashion. Applications,
including bone, tendon, skin,
cardiovascular, and other types of tissue
engineering, can be realized using material
extrusion processes. In addition, extrusion
processes enable adjustable pressure
settings to accommodate the processing
of materials with a range of viscosities [2].
Such recent advances in bioprinting have
significantly affected the development
of potentially new applications for tissue
engineering and regenerative medicine
Q5 (Figure 1).Bacterial polysaccharides have emerged
as a key component of many of the inks
used in bioprinting [3]. These bacterial
polysaccharides can influence key features,
such as the mechanical and thermal
properties, printability, biocompatibility,
and biodegradability. However, implanting
any foreign structure in the body comes
with an increased risk of bacterial infection
and, in particular, bacterial colonization of
the implant itself [4]. Pathogenic bacteria
can form communities called biofilms on
these implanted structures and, when
growing in a biofilm, bacteria are more
tolerant to the rigors of the host immune
system and antimicrobial therapy. Most
hospital-related bacterial infections involvebiofilm formation, with bacteria attaching
to implanted foreign objects, such as
prosthetic joints, dental implants, catheters,
or intravenous lines, being a leading
cause of morbidity [4]. Integrating bacterial
polysaccharides with native anti-infective
properties into bioink formulations can
reduce the risk of infection and have a
role in removing a key barrier to the further
uptake of 3D bioprinting technology within
the biomedical sector. Anti-infective
polysaccharides can also ease some of the
pressure on the healthcare system caused
by antibiotic-resistant infections. 6061 **Bioactive Bacterial**
62 **Polysaccharides**63 Bacteria are rich reservoirs for polysac-
64 charides and, while the primary use of
65 bacterial polysaccharides in bioprinting is
66 to confer structural properties [3], many
67 have been shown to have secondary func-
68 tionalities. An increasingly diverse array of
69 bacterial polysaccharides has been identified
70 that display antibiofilm activity both
71 *in vitro* and *in vivo*. The functional capacity
72 of these polysaccharides to inhibit bacterial
73 adhesion and subsequent biofilm formation
74 has been proposed to be a key
75 competitive strategy to allow a producer
76 species to occupy a given environmental
77 niche [5].The structural variety seen in these
antibiofilm polysaccharides is diverse,
ranging from monosaccharide to hetero-
polysaccharide polymers, with no consistent
feature linked to antibiofilm activity.
Both exopolysaccharides and capsular
polysaccharides have been identified with
antibiofilm activity [6]. Most antibiofilm
polysaccharides identified so far have
broad-spectrum activity against both clinically
relevant Gram-positive and Gram-negative
pathogens. Critically, this activity is
mediated without impacting growth,
ruling this out as a mechanism for their
antibiofilm properties. Potential mechanisms
of action include biomasking, signal
disruption, gene expression disruption, 94



Trends in Biotechnology

Figure 1. Role of Bioactive Bacterial Polysaccharides in Bioprinting. Functional bacterial polysaccharides can be integrated into current bioink formations to confer antibiofilm or antibacterial activities to 3D bioprinted structures, such as bioprinted bone grafts or prosthetic implants. Integrating these bioactive polysaccharides can reduce the probability of implant reject by preventing bacterial attachment and biofilm formation. Depending on the proposed implantation site, integrating probiotic bacteria into bioprinted structures can facilitate targeted probiotic delivery.

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123 and alteration of biotic/abiotic surface
124 properties [5]. Biomasking is the ability
125 of a bacterial polysaccharide to bind to
126 and occlude native bacterial lectins or
127 sugar-binding proteins that are necessary
128 for biofilm initiation. Indeed, in antibiofilm
129 polysaccharides rich in fucose and fruc-
130 tose, such as EPS1-T14, produced by a
131 marine thermophilic species of *Bacillus*,
132 biomasking may be a potential mecha-
133 nism of action because these are known
134 inhibitors of surface lectins [7]. Signifi-
135 cantly, several bacterial polysaccharides
136 can disperse already established biofilms.
137 This includes a range of glucose-rich
138 polysaccharides secreted by food-borne
139 lactic acid bacteria and EPS273, a poly-
140 saccharide secreted by a marine isolate
141 of *Pseudomonas stutzeri*. The underlying
142 mechanism of action of this biofilm dis-
143 persal activity remains to be uncovered
144 [8,9]. However, this suggests that the
145 biomedical applications for such a poly-
146 saccharide are not purely prophylactic
147 but could be used to control and dis-
148 perse established biofilm-associated
149 infections.

150 Compared with antibiofilm polysaccha-
151 rides, only a few bacterially derived poly-
152 saccharides display antibacterial activity
153 [9,10]. ECP, a polysaccharide derived
154 from *Enterobacter cloacae*, was recently
155 shown to exhibit antibacterial activity
156 against a multidrug-resistant isolate of
157 *E. cloacae*. While the precise mechanism
158 of action of this polysaccharide remains
159 unclear, it significantly damages the cell
160 membrane [10]. Some of these antibiofilm
161 and antibacterial polysaccharides exhibit
162 further biologically relevant activities, such
163 as antioxidant activity and metal ion chela-
164 tion activity [8]. Of the anti-infective
165 polysaccharides identified to date, many
166 can also be incorporated into bioinks
167 because of their high levels of thermosta-
168 bility, pseudoplastic rheology, emulsifying
169 activity, and water solubility [3–5]. Criti-
170 cally, most of these anti-infective polysac-
171 charides retain their eukaryotic biological

inertness and are considered noncytotoxic
[7,8]. Given that antibiofilm polysaccha-
rides are nonbiocidal, the capacity for
evolved resistance to their activity is signifi-
cantly diminished. Indeed, in *Escherichia*
coli, resistance to nonbiocidal antibiofilm
polysaccharides is rare and requires
numerous mutations that significantly alter
the surface physiochemical properties of
the bacteria [11]. However, the potential
for resistance to develop to antibacterial
polysaccharides has yet to be explored.

Limitations

The limited uptake of bacterial polysac-
charides as biomaterials is due, at least
partly, to costly production methods,
difficulty in scalability, and the availability
of cheaper synthetic or plant/algal alterna-
tives. However, the emergence of
bioprinting has led to an increased interest
in bacterial polysaccharides as potential
biomaterials for use in a range of medical
applications (e.g., wound dressings, tis-
sue regeneration, and bone repair). The
capacity for both antibiofilm and antibac-
terial polysaccharides to be functionally
integrated into ink for bioprinting to treat
and prevent infection clearly depends on
further investigating their biophysical prop-
erties. However, they do represent a
diverse panel of anti-infective agents that
can be used to augment the biocompati-
bility of traditional bioinks. Rapid advance-
ments in synthetic biology can be utilized
to overcome the scalability and production
cost issues, whereby the bioactive poly-
saccharide-synthesising gene clusters
can be inserted into synthetic genetic
scaffolds to optimize production in work-
horse bacteria. This synthetic biology
approach may also overcome the issue
of minor variations or polysaccharide
modifications that can occur in native
strains, leading to a loss of homogeneity
and potentially bioactivity. The bacteria
producing these anti-infective polysaccha-
rides could also be functionally integrated
into the bioink itself. Similar methodologies
have been used to functionalize a bioink

by integrating strains of bacteria capable
of degrading pollutants or producing
cellulose into already established bioink
formulations. These inks can then be printed
over a given surface in a bespoke geome-
try and incubated for a defined period
to achieve a desired outcome, such as
bioremediation or the formation of a cellu-
lose-based synthetic skin scaffold [12].

Future Directions

The advent of 4D bioprinting, where the
added fourth dimension is the capacity
to alter the shape of a 3D printed structure
over time or exposure to specific stimuli,
also has the potential to transform
bioprinting and to have a key role in tack-
ling bacterial infections in the future.
Hydrogels have already been developed
that have shape-morphing capacity [13].
This technology could be used to create
programmable wound dressings compris-
ing antibiofilm polysaccharides that re-
lease antimicrobials upon exposure to the
molecular determinants associated with
a specific pathogen. However, for this
to be implemented, a new mathematical
modeling approach is necessary to strate-
gically control the sequence of stimulus to
act on the stimulus-responsive material
and, consequentially, for targeted drug
delivery [14]. 3D printed bioinks could
also be used as vectors to influence the
microbiome. Constructing scaffolds or
seeder population reservoirs that can
be implanted into locations such as the
gut during procedures such as bariatric
surgery might pave the way for intelligent
microbiota delivery systems. Bioinks
need to be regarded not only as a vehicle
for cells, but also as being equally im-
portant to the cells themselves in terms
of biological impact; the drive to use
inert polysaccharides will be superseded
by the need for polysaccharides with
additional bioactivities, such as antibac-
terial, antibiofilm, antioxidant, immuno-
stimulatory, or metal chelation activity
[8,15]. Thus, integrating anti-infective poly-
saccharides into bioprinting technology

221 has the potential to reduce the incidence
222 of implant infection in the clinic and miti-
223 gate the spread of antibiotic-resistant
224 isolates.

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References

1. Mandrycky, C. *et al.* (2016) 3D bioprinting for engineering complex tissues. *Biotechnol. Adv.* 34, 422–434
2. Lee, J.M. *et al.* (2018) 3D bioprinting processes: a perspective on classification and terminology. *Int. J. Bioprint.* 4, 151
3. Aljohani, W. *et al.* (2018) Three-dimensional printing of alginate-gelatin-agar scaffolds using free-form motor assisted microsyringe extrusion system. *J. Polym. Res.* 25, 62
4. Bjamsholt, T. *et al.* (2018) Biofilm formation - what we can learn from recent developments. *J. Intern. Med.* 284, 332–345
5. Rendueles, O. *et al.* (2013) Antibiofilm polysaccharides. *Environ. Microbiol.* 15, 334–346
6. Goncalves, M. dos S. *et al.* (2014) Anti-biofilm activity: a function of *Klebsiella pneumoniae* capsular polysaccharide. *PLoS One* 9, e99995
7. Spanò, A. *et al.* (2016) In vitro antibiofilm activity of an exopolysaccharide from the marine thermophilic *Bacillus licheniformis* T14. *Curr. Microbiol.* 72, 518–528
8. Wu, S. *et al.* (2016) Antibiofilm and anti-infection of a marine bacterial exopolysaccharide against *Pseudomonas aeruginosa*. *Front. Microbiol.* 7, 102
9. Abid, Y. *et al.* (2018) Production and structural characterization of exopolysaccharides from newly isolated probiotic lactic acid bacteria. *Int. J. Biol. Macromol.* 108, 719–728
10. Liu, J. *et al.* (2018) Structural investigation of a polysaccharide from the mycelium of *Enterobacter cloacae* and its antibacterial activity against extensively drug-resistant *E. cloacae* producing SHV-12 extended-spectrum β -lactamase. *Carbohydr. Polym.* 195, 444–452
11. Travier, L. *et al.* (2013) *Escherichia coli* resistance to nonbiocidal antibiofilm polysaccharides is rare and mediated by multiple mutations leading to surface physicochemical modifications. *Antimicrob. Agents Chemother.* 57, 3960–3968
12. Schaffner, M. *et al.* (2017) 3D printing of bacteria into functional complex materials. *Sci. Adv.* 3, eaao6804
13. Kirillova, A. *et al.* (2017) 4D biofabrication using shape-morphing hydrogels. *Adv. Mater. Weinheim* 29, 1703443
14. Loh, G.H. *et al.* (2018) An overview of functionally graded additive manufacturing. *Addit. Manuf.* 23, 34–44
15. McCarthy, R.R. *et al.* (2017) Cyclic-di-GMP regulates lipopolysaccharide modification and contributes to *Pseudomonas aeruginosa* immune evasion. *Nat. Microbiol.* 2, 17027