

1 **General estimates of the energy cost of walking in people with different levels and causes of**
2 **lower limb amputation: a systematic review and meta-analysis**

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14

15 **Abstract**

16 *Background:* Energy cost of walking (ECw) is an important determinant of walking ability in people with a
17 lower limb amputation. Large variety in estimates of ECw has been reported, likely due to the heterogeneity of
18 this population in terms of level and cause of amputation and walking speed.

19 *Objectives:* To assess (1) differences in ECw between people with and without a lower limb amputation, and
20 between people with different levels and causes of amputation, and (2) the association between ECw and
21 walking speed.

22 *Study Design:* Systematic review and meta-analysis.

23 *Methods:* We included studies that compared ECw in people with and without a lower limb amputation. A meta-
24 analysis was done to compare ECw between both groups, and between different levels and causes of
25 amputation. A second analysis investigated the association between self-selected walking speed and ECw in
26 people with an amputation.

27 *Results:* Out of 526 identified articles, 25 were included in the meta-analysis and an additional 30 in the walking
28 speed analysis. Overall, people with a lower limb amputation have significantly higher ECw compared to people
29 without an amputation. People with vascular transfemoral amputations showed the greatest difference (+102%)
30 in ECw. The smallest difference (+12%) was found for people with non-vascular transtibial amputations.
31 Slower self-selected walking speed was associated with substantial increases in ECw.

32 *Conclusion:* This study provides general estimates on the ECw in people with a lower limb amputation,
33 quantifying the differences as a function of level and cause of amputation, as well as the relationship with
34 walking speed.

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36 Abstract word count: 249 words

37 **Key words:** energy cost of walking, lower limb amputation, prosthesis, aetiology, level, walking speed

38

39 **Background**

40

41 In the Netherlands, the incidence of lower limb amputations is 20 per 100,000 population.¹ Each year, about
42 3,200 lower limb amputations are performed.² The group of people with a lower limb amputation is
43 heterogeneous, including persons with different levels and causes of amputation and concomitant factors. This
44 heterogeneity is considered a main contributor to differences in the level of functioning between persons with a
45 lower limb amputation.³ Level of amputation can be roughly divided into amputations below and above the knee,
46 with transtibial and transfemoral amputations being the most common. The etiology of amputation can be
47 roughly divided into vascular causes and non-vascular causes. Generally, lower limb amputations with a vascular
48 cause are performed in older persons with medical comorbidities including diabetes, whereas lower limb
49 amputations due to non-vascular causes often include younger persons with fewer comorbidities.⁴ It has been
50 established that both level and cause of amputation have a major effect on walking ability in people with a lower
51 limb amputation.^{3, 5-7}

52

53 Walking ability in people with a lower limb amputation is often assessed in terms of energy cost of walking
54 (ECw). ECw has shown to be related to quality of life and participation in social activities.⁸ It has frequently
55 been found that people with a lower limb amputation have increased ECw compared to persons without an
56 amputation.⁶ After undergoing lower limb amputation, one can choose to walk with or without use of a
57 prosthesis, which will both increase the ECw.⁶ Walking without a prosthesis results in the highest ECw, as
58 additional energy is needed to support body weight on crutches. Walking with a prosthesis also results in greater
59 ECw, as the economy of gait is constrained by the prosthesis. People walking with a prosthesis show reduced
60 ankle push-off power resulting from a reduced ability to plantar flex their ankle. Consequently, people with a
61 lower limb amputation need to use other, less efficient, strategies for propulsion and leg swing.⁹⁻¹¹ Impaired
62 balance control is considered another factor contributing to increased ECw while walking with a prosthesis.^{7, 12}
63 People with a lower limb prosthesis are known to be less stable during steady-state walking compared to people
64 without an amputation.^{12, 13} This requires the use of compensatory strategies in order to maintain balance,
65 resulting in increased energy demands.^{12, 14-16}

66

67 Over the last fifty years, many studies have investigated the ECw in people with a lower limb amputation. The
68 seminal study of Waters et al.⁶ was one of the first studies to systematically investigate the ECw for people with

69 different levels and causes of amputation. Results showed that the ECw in people with a lower limb amputation
70 is dependent on both level and cause of amputation. They reported increases of 25% and 55% in ECw, for
71 persons with a non-vascular amputation at the transtibial and transfemoral level respectively, compared to
72 persons without an amputation. For persons with a vascular amputation, the reported values were even higher,
73 with increases of 65% and 120% for persons with a transtibial and transfemoral amputation respectively. These
74 values as reported by Waters et al.⁶ - and re-evaluated in a later review¹⁷ - are still often used as reference values
75 in clinical practice, since the study of Waters et al. is actually the only study that systematically compared ECw
76 in subgroups stratified for all levels and causes of amputation within one study. However, it can be questioned
77 whether the values provided by Waters et al.^{6, 17} are applicable to the current population of people with a lower
78 limb amputation, as the sample size in the study was rather small (approximately 15 persons for each subgroup
79 of people with an amputation and 5 people without an amputation) to generalize results to the whole population
80 of persons with a lower limb amputation, which might limit precision of the provided estimates. Moreover,
81 patient characteristics, prosthetic developments and assessment methods may have changed over time. ..

82

83 In the years following the seminal research of Waters et al.⁶, the ECw for people with a lower limb amputation
84 has been assessed in many other studies.^{9, 18-20} However, these studies have predominantly focused on one
85 specific cause or level of amputation.^{9, 18-20} In addition, a great variety of types of prostheses has been analysed,
86 as ECw has often been used as an outcome to test a newly developed prosthesis.^{21, 22} Few of these studies
87 included a control group of people without an amputation. Moreover, studies differ in their experimental
88 protocol, using different walking speeds and walking surfaces.^{23, 24} Walking speed has been shown to
89 substantially influence ECw, both in people with and without lower limb amputation.²⁵ ECw is known to have a
90 U-shaped relation with walking speed, increasing at both slow and fast walking speeds.²⁵ It has been shown that,
91 in contrast to persons without an amputation, people with a lower limb amputation walk at speeds slower than
92 their most economic speed.²⁶ Therefore differences in self-selected walking speed can be associated with
93 differences between individuals and subgroups. This can be controlled by studies that use a fixed imposed
94 walking speed rather than self-selected walking speed in order to assess the ECw. However, these ECw
95 outcomes are not representative for walking in daily life.

96

97 Hence, despite the availability of a large (and still growing) amount of quantitative data on the ECw with a lower
98 limb prosthesis, general estimates on the magnitude of the difference in energy cost relative to walking in

99 persons without a lower limb amputation are difficult to derive from the available data due to the heterogeneity
100 between study populations and designs. Still, clinical practice and prosthetic developments need such
101 information in order to set patient-specific expectations for ECw and to develop benchmarks and interventions to
102 reduce the ECw. Therefore, the purpose of this study is to compare the ECw between people with and without a
103 lower limb amputation, and to assess to what extent ECw differs as a function of level and cause of amputation.
104 In addition, we investigated the association between self-selected walking speed and ECw of people with a
105 lower limb amputation, in order to assess how self-selected walking speed might account for the variation in
106 energy cost between and within subgroups.

107

108 **Methods**

109

110 *Search strategy*

111 We performed an electronic search via the following databases until March 2020: PubMed, Physiotherapy
112 Evidence Database (PEDro) and Cumulative Index to Nursing and Allied Health Literature (CINAHL). A
113 detailed description of the applied search strategy is provided in Appendix 1. Searches were pre-limited using the
114 following criteria: English language and abstract available. Articles were further selected by reading title and
115 abstract, after which a final selection was made based on the full article. Articles were selected for two types of
116 analysis. In *analysis 1*, we compared the ECw between people with a lower limb amputation, stratified for level
117 (transtibial vs. transfemoral) and cause (vascular vs. non-vascular) of amputation, and persons without an
118 amputation. In *analysis 2*, we assessed the effect of self-selected walking speed on ECw. Articles selected for
119 *analysis 2* did not need to include people without an amputation. All included articles needed to provide explicit
120 data concerning average and standard deviation of ECw and walking speed and meet all other inclusion criteria
121 described below. When an article had been selected for either *analysis 1* or *analysis 2*, but did not provide all
122 required details, the author was approached to provide the exact data. One author (XX) selected articles and
123 extracted data. Another author (YY), checked the selection and data extraction of all articles. If discrepancies
124 existed, the authors conferred to reach consensus on the specific issue.

125

126 *Inclusion criteria*

127 The following inclusion criteria were used when selecting studies: 1) participants are at least 18 years of age; 2)
128 inclusion of a control group without amputation (*analysis 1* only); 3) inclusion of participants with transtibial or

129 transfemoral amputation; 4) measurement of energy consumption during walking (for people with an
130 amputation: during walking with prosthesis); 5) energy consumption measured by indirect calorimetry; 6) the
131 article is not a case-study or a review article.

132

133 *Data extraction, outcome measures and risk of bias assessment*

134 The following information was extracted from the selected articles: 1) subject characteristics (e.g., age, gender);
135 2) level of amputation; 3) cause of amputation; 4) system used for measuring oxygen consumption and
136 calculation of the ECw; 5) type of prosthetic component used; 6) study design (instructions, duration and
137 environment); 7) ECw; 8) walking speed at which ECw was assessed.

138

139 When an article investigated the ECw for a group of people with mixed levels and/or causes of amputation, the
140 author was approached to provide additional information needed to subgroup persons according to the level and
141 cause of amputation. Subgroups with fewer than three participants were excluded from further analysis. When a
142 particular study tested multiple types of prostheses in the same group of participants, the ECw and walking speed
143 related to the prosthesis with the most widespread clinical use at the time of the study were used for further
144 analysis (see Appendix 2 for detailed selection, not chosen options are provided in italics). The prosthesis with
145 most widespread clinical use was selected by one author with longstanding experience in the field (YY). In the
146 case that ECw had been assessed during both overground and treadmill walking, we used the ECw during
147 overground walking for further analysis, as this most closely resembles walking in daily life.²⁷ For each study,
148 one combination of walking speed and ECw was used for analysis. If ECw had been assessed both at imposed
149 and self-selected walking speeds, we used ECw values at self-selected walking speed for further analysis.
150 Furthermore, when ECw had been measured only at multiple imposed walking speeds, we selected the ECw
151 associated with the walking speed that was closest to the average self-selected walking speed of the specific
152 subgroup. Average self-selected walking speed for each specific subgroup was based on the preferred walking
153 speed found in other selected studies: transfemoral vascular: 0.52 m s⁻¹; transfemoral non-vascular: 1.00 m s⁻¹;
154 transtibial vascular: 0.79 m s⁻¹; transtibial non-vascular: 1.34 m s⁻¹. Summary information regarding study
155 protocols of included studies is presented in Appendix 3.

156

157 Two of the reviewers (XX, ZZ) independently assessed the risk of bias of the included studies with the
158 Newcastle-Ottawa Scale (NOS²⁸), which was modified for the study purpose (see Appendix 4). The NOS

159 contains items on participant selection, comparability of the study groups and outcome assessment. The scale
160 ranges from 0-11 for *analysis 1* and from 0-7 for *analysis 2*, as comparability items were not relevant for
161 *analysis 2*. Higher NOS-scores reflect a lower risk of bias.

162 *Energy cost calculations*

163 In this study, we analysed the gross metabolic EC_w expressed in ml O₂ kg⁻¹ m⁻¹. When studies only reported
164 oxygen consumption ($\dot{V}O_2$; ml O₂ kg⁻¹ min⁻¹), EC_w was calculated by dividing oxygen consumption by walking
165 speed (in m min⁻¹). When actual metabolic energy expenditure ($\dot{E}E$) was provided in J kg⁻¹ s⁻¹ it was converted
166 into ml O₂ kg⁻¹ m⁻¹ according to Equation (1), with walking speed (v) expressed in m min⁻¹. Respiratory exchange
167 ratio (RER) was assumed to be equal to 1.²⁹

$$EC_w = \frac{\dot{E}E \times 60 \times v}{(4.940 \times RER + 16.040)} \quad (1)$$

168 *Meta-analysis calculations*

169 In order to perform a meta-analysis with the data collected for *analysis 1*, the standard deviation (SD) of EC_w
170 was needed. When articles did not report SD, 95% confidence interval was used to determine SD, according to
171 Equation (2). Studies to which Equation (2) was applied are indicated with an asterisk (*) in Appendix 2. When
172 articles did not report SD nor 95% CI and when this data could not be retrieved from the original author, articles
173 were excluded from *analysis 1*.

174

$$SD = \frac{\sqrt{N} \times (\text{upper limit 95\% CI} - \text{lower limit 95\% CI})}{3.92} \quad (2)$$

175

176 *Meta-analysis*

177 Meta-analyses were carried out with RevMan 5.3 (The Nordic Cochrane Centre, Copenhagen, Denmark). Since
178 all included studies used the same outcome measure with similar (or converted to similar) units of measurement,
179 data were pooled using the mean difference (MD). Significance level was set at p<0.05. Random effects models
180 were used (as a high level of heterogeneity was evident, and > 5 studies were available). Statistical heterogeneity
181 was confirmed by visual inspection of the forest plots, and with the I²-statistic, with heterogeneity considered to

182 be present if χ^2 was significant ($p < 0.1$).³⁰ We sub grouped studies according to the level (transtibial vs.
183 transfemoral) and cause (vascular vs. non-vascular) of amputation, to assess if ECw would be different for
184 people with different combinations of levels and causes of amputation. When an article provided data for
185 different subgroups of persons (i.e. different levels/causes of amputation) but for just one single control group,
186 the means and SDs for this particular control group were used as many times in the same analysis, but we
187 divided the sample size by the number of comparisons it was included in.³⁰

188

189 *Analysis of walking speed*

190 The relationship between walking speed and ECw was analysed descriptively by fitting a polynomial through
191 the available data of ECw and self-selected walking speed of different subgroups. The curves were second-order
192 polynomial fits through all data points of a specific subgroup, which were described by the function:
193 $ECw = av^2 + bv + c$. Walking speed was expressed in $m\ s^{-1}$. For each study, only one specific estimate of
194 ECw (i.e. at actual or approximated self-selected walking speed) was added to this analysis. These analyses were
195 performed in Matlab (The Mathworks, Natick, MA, USA) using the function *polyfit*.

196

197

198 **Results**

199 *3.1 Literature search*

200 Figure 1 shows the flow of study selection. In total, our search identified 526 articles. After screening of titles
201 and abstracts, 40 potential articles were selected for *analysis 1* and 87 additional potential articles for *analysis 2*.
202 Application of the in- and exclusion criteria eventually resulted in the inclusion of 35 articles in *analysis 1* and
203 41 additional articles in *analysis 2*. Most common reasons for exclusion at this stage were: unavailability of full
204 text paper, measurement of energy consumption by other means than indirect calorimetry, and data for a group
205 of persons that had already been presented in an earlier published article that was already included (see Figure
206 1). Regarding *analysis 1*, the results of 10 articles were only descriptively synthesised, but not included in the
207 meta-analysis. Reasons for this were that the required data could not be extracted reliably and missing data could
208 not be obtained by contacting the authors³¹⁻³⁶ (N=6), that standard deviations could not be obtained^{20, 37} (N=2),
209 outlying data (extremely high ECw values³⁸; N=1), or analysis of ECw in the presence of external stimuli³⁹
210 (N=1; referred to as 'other' in Figure 1). In *analysis 2*, 11 articles were fully excluded from analysis, because no
211 accurate data extraction was possible (N=11).

212

213 In sum, we selected 25 articles for the meta-analyses in *analysis 1* and 30 additional articles for the walking
214 speed analysis in *analysis 2*.

215

216 **[insert Figure 1]**

217

218 *3.2 Study characteristics*

219 *3.2.1 Participants characteristics*

220 In total, 367 persons with a lower limb amputation and 282 persons without an amputation participated in the
221 selected articles for *analysis 1* and 362 additional persons with a lower limb amputation participated in the
222 selected articles for *analysis 2*. Table 1 shows the number and type of specific subgroups that were described in
223 the included articles for analysis 1 and 2. Most of the included articles investigated persons with a non-vascular
224 transtibial or transfemoral amputation. Considerable heterogeneity was noted in terms of participants'
225 characteristics, such as mean age (range controls: 23–60 years; range people with amputation; 22-73 years),
226 gender (85% male), walking speed (range controls: 0.83–1.56 m s⁻¹; range people with amputation: 0.45–1.50 m

227 s⁻¹) and time since amputation (range: 9 weeks–31 years). For details for each of the studies, please see the
228 overview tables in Appendix 2 and Appendix 3.

229 **[insert Table 1]**
230

231 3.2.2 Experimental protocol

232 In *analysis 1*, 18 articles assessed ECw using preferred walking speed, whereas 7 articles used an imposed fixed
233 walking speed. Regarding walking surface, 12 articles performed their measurements on a treadmill and 13
234 articles performed overground measurements, either indoor or outdoor. In *analysis 2*, 20 articles studied ECw
235 while walking at preferred walking speed, whereas 10 articles studied ECw at an imposed fixed speed. In
236 *analysis 2*, 20 articles investigated ECw using a treadmill and 10 articles investigated ECw during overground
237 walking. The duration of the walking trials varied between 2 and 20 minutes. All studies, except for two, did
238 report the requirement of steady state walking. In both *analysis 1* and *analysis 2*, 14 studies used the average
239 value over the last 2 or 3 minutes of their walking trials for analysis of the energy cost. Other studies took the
240 average over shorter time periods, whereas 2 studies in *analysis 1* and 3 studies in *analysis 2* did not provide clear
241 information about the use of averaging methods when calculating the energy cost.

242

243 3.3 Risk of bias assessment

244 Appendix 5 shows the NOS-scores of each study for *analysis 1 and 2*. Mean score and standard deviation were
245 6.4 ± 2.2 (range: 2-9) for *analysis 1*, and 4.5 ± 0.9 (range: 2-6) for *analysis 2*. For most studies, stars were
246 awarded for clear descriptions of the study groups and the applied protocol. Overall, stars were often withheld
247 for items relating to the selection and follow-up of study groups, as this was often not explicitly described. In
248 *analysis 1*, comparability of the groups was often achieved in terms of age and sex of the participants, but only in
249 a few studies were groups comparable in terms of physical fitness or physical activity levels.

250

251 3.4 Data analysis

252 3.4.1 Meta-analyses

253 A total of 25 studies (describing 37 comparisons) were included in the meta-analysis that investigated the
254 difference in ECw between people with and without an amputation at self-selected walking speed. Results
255 showed that persons without an amputation overall have significantly lower ECw compared to people with a
256 lower limb amputation (MD=0.06 ml O₂ kg⁻¹ m⁻¹, 95% CI=[0.04; 0.07], Z=8.80, $p<0.001$; see Figure 2).

257 Considerable heterogeneity was present ($I^2=88\%$). Subgroup analyses revealed that the difference in ECw was
258 significantly different as a function of levels and causes of amputation ($\chi^2(3)=165.92$, $p<.001$, $I^2=98.2\%$). ECw
259 was significantly higher compared to controls in all four subgroups (see Figure 2). The highest ECw was
260 observed for people with a vascular transfemoral amputation (MD=0.18 ml O₂ kg⁻¹ m⁻¹, 95% CI=[0.16, 0.21]),
261 followed by the non-vascular transfemoral group (MD=0.07 ml O₂ kg⁻¹ m⁻¹, 95% CI=[0.06, 0.08]), the vascular
262 transtibial group (MD=0.06 ml O₂ kg⁻¹ m⁻¹, 95% CI=[0.03, 0.09]), while the smallest (yet still significant)
263 difference in ECw was observed for the non-vascular transtibial group (MD=0.02 ml O₂ kg⁻¹ m⁻¹, 95% CI=[0.01,
264 0.03]). As can be seen in Table 2, the increase in ECw was significantly different between all subgroups ($p\leq.02$),
265 except for the comparison of the non-vascular transfemoral group and vascular transtibial group ($p=.58$).

266

267 When expressed as a percentage of the weighted average of ECw of the respective control groups, the ECw for
268 people with a lower limb amputation at self-selected walking speed was 35% higher compared to people without
269 an amputation. When separately assessed for each of the subgroups, ECw values were 12% higher for the non-
270 vascular transtibial group, 36% for the vascular transtibial group, 41% for the non-vascular transfemoral group,
271 and 102% for the vascular transfemoral group.

272

273 **[insert Figure 2]**

274

275 **[insert Table 2]**

276 *3.4.2 Descriptive synthesis*

277 We descriptively synthesized the results of the 10 articles that were excluded from the meta-analysis, because no
278 reliable data extraction was possible. All of the excluded articles investigated the ECw related to level of
279 amputation, and did not directly compare groups with different causes. Most of the articles showed results that
280 were similar to the results found in the meta-analysis. Do Nascimento Garcia et al.,³⁸ Herr and Grabowski,³⁶
281 Gailey et al.,²⁰ Jaegers et al.,³³ Schnall et al.,³⁹ and Ladlow et al.³⁵ all showed significant increases in ECw for
282 persons with a non-vascular amputation at the transtibial or transfemoral level compared to persons without an
283 amputation, with the largest increase found for persons with a transfemoral amputation. This result was also
284 found by Ganguli et al.,³² but they did not report any significance values. Similar results were reported by Pinzur
285 et al.,³⁷ in people with vascular transtibial and transfemoral amputations, but they did not report significance
286 values either. The studies of Kark et al.³⁴ and Eckard et al.³¹ seemed to deviate slightly from the results in the

287 meta-analysis. Kark et al.³⁴ investigated ECw in transtibial amputees and transfemoral amputees with different
288 causes of amputation, but only found significantly increased ECw for transfemoral amputees compared to people
289 without an amputation. Eckard et al.³¹ did not find any differences in ECw in a group consisting of both people
290 with transtibial and transfemoral non-vascular amputations compared to persons without an amputation.

291

292 *3.4.3 The relation between ECw and self-selected walking speed*

293 Figure 3 shows the association between self-selected walking speed and ECw across different causes and levels
294 of amputation and people without an amputation. Average preferred walking speed for each group was as
295 follows; transfemoral vascular: $0.62 \pm 0.11 \text{ m s}^{-1}$; transfemoral non-vascular: $1.02 \pm 0.20 \text{ m s}^{-1}$; transtibial
296 vascular: $0.82 \pm 0.15 \text{ m s}^{-1}$; transtibial non-vascular: $1.20 \pm 0.51 \text{ m s}^{-1}$. Results indicate that ECw is moderately
297 to strongly associated with self-selected walking speed in all subgroups, as shown by the R^2 values. It can be
298 observed that especially persons with an amputation due to vascular reasons generally walk below their most
299 economic walking speed, which contributes to their increase in ECw compared to persons without an
300 amputation. Note that the variation in ECw that could be accounted for by differences in walking speed (i.e. a
301 shift of a specific group on their speed-ECw curve to the left ascending flank) seems substantial relative to the
302 variation accounted for by cause or level of amputation alone (i.e. an upward shift of the speed-ECw curves
303 between groups).

304

305 **[insert Figure 3]**

306 **Discussion**

307 The aim of this study was to provide quantitative estimates of differences in ECw between people with and
308 without a lower limb amputation and to investigate the influence of cause of amputation, level of amputation and
309 walking speed using a systematic review and meta-analysis of previous literature. In agreement with our
310 expectations and previous research,⁶ the results of this study showed that ECw is significantly higher in people
311 with an amputation who walk with a lower limb prosthesis compared to people without an amputation (35%). On
312 average, the difference in ECw is most pronounced in people with a transfemoral amputation due to vascular
313 reasons (102%), followed by non-vascular transfemoral amputation (41%), vascular transtibial amputation (36%)
314 and lowest after non-vascular transtibial amputation (12%). Furthermore, results suggest that reductions in self-
315 selected walking speed seem to be a major contributor to the higher ECw in people with an amputation.

316 In total, we included 25 articles in the meta-analysis, which described 37 comparisons between designated
317 subgroups of people with a lower limb amputation and people without an amputation. These comparisons were,
318 however, not distributed equally between subgroups. Specifically, people with amputations due to vascular
319 problems were under-represented in literature. Only four articles in the meta-analysis investigated ECw for
320 persons with a vascular amputation, together including 47 persons with an amputation. From these articles data
321 on three vascular-transfemoral groups (n=23) and three vascular-transfemoral groups (n=24) could be derived. It
322 should be acknowledged that this limited amount of data reduces the reliability of the estimates for these
323 subgroups. Please note that most articles that were only included in the descriptive synthesis showed similar
324 results to those in the meta-analysis, both in terms of ECw as in terms of relative underrepresentation of people
325 with vascular amputation.

326

327 Generally, the results of our meta-analysis are in agreement with the study of Waters et al.,⁶ as both studies
328 indicate the highest ECw for persons with a vascular transfemoral amputation and the lowest ECw for non-
329 vascular transfemoral amputations. Although the current meta-analysis shows that people with an amputation have
330 higher ECw compared to people without an amputation these differences were smaller than those reported by
331 Waters et al.⁶ Waters et al.⁶ reported the highest ECw values amongst all included studies for each single
332 subgroup of people with an amputation. Where Waters et al.⁶ reported an increase between 25 and 120%, we
333 found an average increase between 12 and 102%. This overestimation could be a result from the relatively small
334 population studied by Waters et al.,⁶ which might not have been fully representative for the general population of
335 people with a lower limb amputation. Additionally, improved rehabilitation and/or prosthetic technology in
336 recent years may have contributed to these different estimates. Worthy of note, however, no clear trend between
337 year of publication and differences in energy cost can be observed among the included studies (Fig 2). Albeit
338 that we only included studies at self-selected comfortable walking speed while the advantages of some modern
339 prostheses have been shown to be more apparent at slow or high walking speeds.⁴⁰

340

341 Our results show that self-selected walking speed partly accounts for the higher ECw in people with a lower limb
342 amputation. The relation between walking speed and ECw can be modelled as a U-shaped function.^{41, 42} For
343 healthy individuals without an amputation costs are minimal around 1.2 m s⁻¹ but rise rapidly at lower and faster
344 walking speeds. Figure 3 provides additional insight in the effect of walking speed on ECw by visualising the
345 position of the curves of all subgroups relative to each other. The coefficients of these curves do not have a

346 physiological meaning, but only serve to describe the relationship between self-selected walking speed and ECw
347 for each of the subgroups. It is expected that the speed-ECw curves of people with a lower limb amputation are
348 shifted upwards as a consequence of reduced gait economy.²⁵ Figure 3 demonstrates that irrespective of such an
349 upward shift, a substantial part of the difference in ECw at self-selected walking speed is due to the fact that
350 people with a lower limb amputation, and especially those with a vascular cause of amputation, walk at slow
351 speeds on the steeply ascending side of the speed-ECw curve. Hence, differences in ECw at self-selected
352 walking speed between groups could partly be explained by their lower self-selected walking speeds, next to the
353 upward shift of the speed-ECw curve. Note that an accurate analysis of the speed-ECw curves could not be
354 performed in this study as data of subgroups were not available over comparable and full ranges of the walking
355 speed spectrum. Therefore, we cannot draw definitive conclusions on the potential upward shift or shift in most
356 economic speed for these subgroups.

357

358 Previous studies have shown that for people with a lower limb amputation, especially those with vascular cause
359 of amputation and transfemoral amputation, preferred walking speed is generally slower than their most
360 economic speed.^{25, 26} People might reduce speed due to balance problems and associated fear of falling,⁴³ but it
361 has been shown that the reduction in walking speed might also be related to energetic limitations. People with a
362 lower limb amputation generally have a reduced aerobic capacity, especially people with a vascular cause of
363 amputation.⁴⁴ The combination of reduced capacity and high demand increases the relative aerobic load at a
364 given walking speed, which is known to affect quality of life in people with a lower limb amputation.⁸ Reducing
365 self-selected walking speed may therefore be necessary to maintain aerobic load within sustainable limits, i.e. at
366 an acceptable percentage of maximal aerobic capacity.^{6, 26} Yet this comes at the expense of walking economy.
367 Consequently, next to level and cause of amputation, self-selected walking speed (and underlying factors such as
368 physical fitness and fear of falling) needs to be taken into account as an important predictor of the ECw of
369 individuals with lower limb amputation.

370

371 Our current review complements recent work by van Schaik et al.,⁴⁵ who performed a systematic review and
372 meta-analysis of the metabolic requirement of daily activities, including walking, in people with lower limb
373 amputation. In contrast to our analysis, this earlier study used energy consumption per unit of time ($\text{ml O}_2 \text{ kg}^{-1}$
374 min^{-1}) as outcome of interest. In agreement with our results they found a significant effect of level of amputation
375 on energy requirement of walking, but no effect of cause of amputation was found. This was attributed to the low

376 number of studies reporting on people with vascular cause of amputation. Van Schaik et al.⁴⁵ showed that
377 walking at slower speeds resulted in lower energy consumption per unit of time – which is in line with the idea
378 that people with a lower limb amputation probably walk slower to reduce the relative aerobic load of walking.
379 However, when energy consumption is expressed per unit of time it is ignored that such a decrease in walking
380 speed reduces walking economy (i.e. energy cost per unit distance). Our current review thus provides further
381 important insights into the effects of reduced preferred walking speed on energy cost of people with different
382 levels and causes of amputation. In addition, we also show how slower self-selected walking speed in persons
383 with an amputation is related to an increase in energy cost, both as function of level and cause of amputation,
384 which was not available in the study by van Schaik et al.⁴⁵

385

386 **Limitations**

387 One main limitation of the current review is the heterogeneity of the included studies in terms of group size,
388 participant characteristics (e.g. age, time since amputation) and study characteristics (e.g. walking speed and
389 duration, treadmill versus overground walking). Our risk of bias assessment highlights the importance of
390 standardising measurement protocols and measuring and reporting possible confounding factors. This
391 heterogeneity– which has also been discussed by others^{7, 45, 46} – could explain the considerable range of estimates
392 for increased ECw at preferred walking speed between studies. Moreover, this heterogeneity may influence the
393 accuracy of our estimates, when factors such as group size, participants and study characteristics were not
394 distributed equally over the different subgroups. Although there were not enough studies available to statistically
395 investigate the effect of such factors, inspection of the included studies did not point to clear systematic
396 differences in these factors between subgroups. Our second limitation is related to converting all outcomes into
397 the same unit. The applied equations included some assumptions about resting metabolism and RER. In
398 Equation (1), RER was assumed to be equal to 1, this value might be slightly too high to achieve during walking
399 for people with an amputation. However, Equation (1) was applied to only 3 studies in *analysis 1* and 6 studies
400 in *analysis 2*. Moreover, effect of lower bound RER values would not exceed 5% in ECw, and would not have
401 affected our overall conclusions. A final limitation pertains to the fact that this systematic review was not
402 prospectively registered with PROSPERO, which would in hindsight have been preferred.

403

404 **Further research**

405 The current meta-analysis provides quantitative estimates of ECw in people with a lower limb amputation with
406 different causality and at different levels. However, the reliability of these results may be affected by the
407 heterogeneity of the studies that were combined. Therefore, future research should clearly report and standardise
408 factors such as walking speed, walking surface and duration of the walking trial. Moreover, the risk of bias
409 assessment shows the importance of reporting possible matching possibly confounding factors such as age and
410 physical fitness when comparing different groups of persons with and without amputations, and of providing
411 detailed information regarding data analysis (i.e. walking at steady-state and calculation of ECw). Related to this,
412 there is a clear need for studies that investigate the interaction of level and cause of amputation and walking
413 speed within a single study. This is essential to better understand the effects of these factors on the ECw after
414 amputation. Furthermore, future research should especially focus on the ECw and walking speed of people with
415 an amputation due to vascular reasons, since data for this specific patient group is scarce while the incidence of
416 dysvascular amputation is the highest of all causes in Western countries. This group is also known to have
417 limited exercise capacity, which compounds the negative effects of high aerobic demand of walking for
418 regaining walking ability.^{26,44}

419

420 **Conclusion**

421 This systematic review provided updated quantitative estimates of energy cost of walking (ECw) of people with
422 a lower limb amputation at their preferred walking speed, stratified for level and cause of amputation. Based on
423 our meta-analysis, differences in ECw of +12% and +41% were found for people with non-vascular transtibial
424 and transfemoral amputations compared to people without an amputation, respectively, and more pronounced
425 differences in ECw were found for people with vascular transtibial (+36%) and transfemoral amputations
426 (+102%). Moreover, our data suggest that a slow preferred walking speed may be a key factor for the observed
427 increase in ECw in people with a lower limb amputation. The estimates provided in this review study can be
428 used as reference values in clinical practice, to improve patient expectations, guide clinical decision making and
429 benchmark prosthetic developments.

430

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432

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437 **Author contribution**

438 XX carried out the data collection, analysis and writing of the article. YY conceived the general idea of this
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440 contributed to writing and proofing the manuscript.

441

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689 **APPENDIX 1 – Search strategy**

#1 - ENERGY COST	Energy AND (Cost OR Consumption OR Expenditure)
#2 - POPULATION	Amputation OR Amputees OR Artificial limbs OR Prosthesis
#3 - GAIT	Walking OR Gait OR Ambulation OR Locomotion
#4 – COMBINED	#1 AND #2 AND #3

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APPENDIX 2 – Overview study populations

Analysis 1

Study	Controls			People with an amputation						
	N	Age (years)	v (m/s)	N	Cause	Level	Age (years)	Gender	v (m/s)	Prosthesis
Carse et al. ⁴⁷	10	51 ± 9	1.41 ± 0.1	8	Vascular	TF	60.8 ± 10.5	-	0.66 ± 0.24	Several types of knee, socket and suspension
				32	Non-vascular	TF	54.0 ± 12.5	-		0.92 ± 0.20
Chin et al. ⁴⁸	14	25.2 ± 4.0	1.50	8	Non-vascular	TF	22.5 ± 3.3	6/2	1.17	Intelligent prosthesis
Esposito et al. ¹⁸	13	26.5 ± 6.0	1.21 ± 0.02	13	Non-vascular	TT	28.9 ± 5.3	13/0	1.20 ± 0.04	Energy storage and return prosthetic foot
Gailey et al. ⁴⁹	10	34.0 ± 12.9	1.27	10	Non-vascular	TT	37.8 ± 10.4	10/0	1.27	-
Gailey et al. ⁵⁰	10	33.2 ± 9.57	1.12	10	Non-vascular	TF	37.2 ± 11.0	10/0	1.12	CAT-CAM socket design
				10	Non-vascular	TF	34.6 ± 9.83	10/0		1.12
Ganguli et al. ⁵¹	16	28.4 ± 7.05	0.83	10	Non-vascular	TT	29.9 ± 11.0	10/0	0.83	Patellar Tendon-Bearing
Gardinier et al. ⁵²	10	48.4 ± 16.62	1.28 ± 0.1	10	Non-vascular	TT	46.5 ± 14.9	10/0	1.28 ± 0.12	Unpowered prosthesis

											<i>Powered prosthesis</i>
Genin et al. ²⁵	13	27.8 ± 5.2	1.41 ± 0.02	9	Non-vascular	TT	35.3 ± 7.2	9/0	1.39 ± 0.17	KMB or Iceross socket	
				10	Non-vascular	TF	34.7 ± 5.1	10/0	1.05 ± 0.05	CAT-CAM or QUAD	
Gitter et al. ⁵³	8	31.8	1.36 ± 0.13	8	Non-vascular	TF	37.3	-	1.20 ± 0.10	-	
Gjovaag et al. ⁵⁴	12	43.0 ± 11.7	1.44 ± 0.13	12	Non-vascular	TF	42.8 ± 13.5	6/6	0.88 ± 0.18	Microprocessor knee joint	
Gjovaag et al. ⁵⁵ *	8	39.0 ± 12.3	1.52 ± 0.15	8	Non-vascular	TF	37.0 ± 10.9	4/4	1.22 ± 0.19	Microcontroller knee joint and Hydraulic knee joint	
Houdijk et al. ⁹	11	47 ± 11	1.52 ± 0.21	3	Vascular	TT	46 ± 9	-	1.31	Dynamic foot	
				8	Non-vascular	TT			1.33		
Hsu et al. ⁵⁶	18	27.5 ± 5.12	1.56	5	Non-vascular	TT	31.6 ± 4.28	5/0	1.34	FlexFoot	
											<i>SACH/ Reflex VSP</i>
Hunter et al. ⁵⁷	10	30.7 ± 5.6	1.34	7	Non-vascular	TT	35.3 ± 5.2	-	1.34	-	
Ijmker et al. ⁵⁸	15	56.7 ± 12.4	1.10 ± 0.13	12	Non-vascular	TF	53.7 ± 13.0	7/4	0.73 ± 0.20	-	
				15	Non-vascular	TT	57.3 ± 13.8	10/2	0.95 ± 0.17	-	

Jarvis et al. ⁵⁹ *	10	30 ± 6	1.29 (1.25-1.33)	10	Non-vascular	TF	29 ± 3	-	1.22 (1.08-1.36)	Hydraulic polycentric knee unit, elastic response foot
				10	Non-vascular	TT	28 ± 4	-	1.36 (1.28-1.44)	Hydraulic polycentric knee unit, elastic
Mengelkoch et al. ²¹	3	35.3 ± 9.0	1.37 ± ???	3	Non-vascular	TT	35.3 ± 10	3/0	1.07 ± ???	SACH foot <i>Renegade/ Nitro ESAR</i>
Mengelkoch et al. ⁶⁰	3	27.0 ± 7.8	1.37 ± ???	3	Non-vascular	TF	27.7 ± 8.1	3/0	0.97 ± ???	SACH foot <i>Renegade/ Nitro ESAR</i>
Paysant et al. ²³	20	39.7	1.52 ± 0.11	10	Non-vascular	TT	39.2	10/0	1.49 ± 0.15	Silicon liners and suspension sleeves, energy storage foot
Russell-Esposito ¹⁹	14	26 ± 6	1.34 ± 0.16	14	Non-vascular	TF	27 ± 5	-	1.23 ± 0.20	Knee: Genium, C-leg, Total Knee; Feet: several types (N=8; Trias, Re-Flex, Re-Flex Rotate, etc.)
Russell-Esposito ⁶¹	8	29.4 ± 3.8	1.19 ± 0.11	8	Non-vascular	TT	32.9 ± 5.7	8/0	1.16 ± 0.09	Passive-dynamic, energy-storage-and-return foot
Russell-Esposito ⁶²	6	23 ± 5	1.21 ± 0.03	6	Non-vascular	TT	29 ± 6	5/1	1.24 ± 0.05	Energy-storage-and-return
Starholm et al. ²⁴	8	39.0 ± 12.3	1.52 ± 0.10	8	Non-vascular	TF	37.0 ± 10.9	4/4	1.22 ± 0.10	Several types of prosthesis (N=6; microprocessor knee, carbon foot etc.)
Waters et al. ⁶	10	Range: 30-70	1.37 ± ???	13	Vascular	TF	60	-	0.60 ± 0.25	Total contact quadrilateral socket
				13	Vascular	TT	63	-	0.75 ± 0.15	Patellar tendon bearing socket

				15	Non-vascular	TF	31	-	0.87 ± 0.23	Total contact quadrilateral socket
				14	Non-vascular	TT	29	-	1.18 ± 0.17	Patellar tendon bearing socket
Wezenberg et al. ²⁶	21	60.80 ± 5.90	1.25 ± 0.15	15	Non-vascular	TT	60.3 ± 7.4	9/6	1.04 ± 0.18	-
				11	Non-vascular	TF	61.4 ± 4.1	10/1	0.86 ± 0.15	-
				7	Vascular	TT	66.9 ± 6.2	6/1	0.73 ± 0.24	-
				3	Vascular	TF	65.0 ± 6.2	2/1	0.63 ± 0.06	-
Analysis 2										
Askew et al. ⁶³				9	Non-vascular	TT	41.3 ± 14.3	9/0	0.98	Dynamic response foot with rigid ankle Dynamic response foot with hydraulic ankle
Barth et al. ⁶⁴				3	Vascular	TT	64	3/0	0.75 ± 0.01	Soft removable liner
				3	Non-vascular	TT	39.3	3/0	1.07 ± 0.06	Soft removable liner
Bell et al. ⁶⁵				10	Non-vascular	TF	32 ± 6.1	Unknown	1.11 ± 0.1	C-leg
				16	Non-vascular	TF			1.28 ± 0.2	C-leg
Bellmann et al. ⁶⁶				9	Non-vascular	TF	35.4 ± 11	7/2	(1.0-1.2)	C-leg

		vascular						
Buckley et al. ⁶⁷	6	Non-vascular	TT	39.5 ± 9.9	6/0	0.89 ± 0.08	Total contact socket	
Buckley et al. ⁶⁸	3	Non-vascular	TF	48.3 ± 10.1	3/0	0.70 ± 0.26	Conventional pneumatic swing phase control mechanism <i>Intelligent prosthesis</i>	
Cao et al. ⁶⁹	6	Non-vascular	TF	36.8 ± 8.1	6/0	1.10	Intelligent prosthesis knee	
Cassillas et al. ⁷⁰	12	Non-vascular	TT	50 ± 13.9	12/0	1.22 ± 0.13	SACH <i>Energy storing and return foot</i>	
	12	Vascular	TT	73 ± 7	10/2	0.58 ± 0.11	SACH <i>Energy storing and return foot</i>	
Darter & Wilken ⁷¹	6	Non-vascular	TT	30 ± 4	5/1	1.34	Customary device	
Darter et al. ⁷²	8	Non-vascular	TF	41.4 ± 12.1	5/3	1.12	Microprocessor knee unit	
Detrembleur et al. ⁷³	7	Vascular	TT	50.5 ± 11	Unknown	0.80 ± 0.42	KMB socket or Iceross sockets with MultiFlex or FlexFoot	
	7	Non-vascular	TF	38.5 ± 12	Unknown	0.67 ± 0.42	CAT-CAM socket or quadrilateral socket, both with various types of knees	
Goktepe et al. ⁷⁴	32	Non-vascular	TT	28.1 ± 5.09	32/0	0.83	Patellar tendon bearing sockets	

Grabowski et al. ⁷⁵	9	Non-vascular	TF	30.1 ± 4.37	9/0	0.83	Quadrilateral of ischial containment socket with suction suspension
	4	Non-vascular	TT	38-39	4/0	1.25	ESAR prosthesis <i>K3 Promotor foot</i>
Graham et al. ⁷⁶	6	Non-vascular	TF	40.3	6/0	1.00	MultiFlex Foot Energy storing and return foot
Houdijk et al. ¹⁶	10	Non-vascular	TT	60.4 ± 18.3	7/3	1.28 ± 0.19	Various types of prosthetic feet, socket and suspension
	6	Vascular	TT	62.8 ± 10.2	6/0	1.02 ± 0.25	Various types of prosthetic feet, socket and suspension
Hsu et al. ⁷⁷	7	Non-vascular	TF	52.1 ± 10.7	7/0	1.21 ± 0.08	Various types of prosthetic feet, knees, socket and suspension
	3	Vascular	TF	59.7 ± 4.9	3/0	0.77 ± 0.35	Various types of prosthetic feet, knees, socket and suspension
Kirker et al. ⁷⁸	8	Non-vascular	TT	36 ± 15	8/0	1.19 ± 0.18	FlexFoot <i>Otto Bock C-Walk Foot/ SACH foot</i>
	6	Non-vascular	TF	36.5 ± 6.2	5/1	1.23 ± 0.17	Pneumatic, swing phase control
Lin-Chan et al. ⁷⁹	8	Non-vascular	TT	36 ± 15	8/0	1.33	60% of intact limb below-knee mass <i>80 or 100% of intact limb below-knee mass</i>

Macfarlane et al. ⁸⁰	5	Non-vascular	TF	36.8 ± 5.07	5/0	1.11	FlexFoot
McDonald et al. ⁸¹	27	Non-vascular	TT	42.3 ± 11	22/5	0.96 ± 0.18	Energy Storing Foot <i>Crossover foot</i>
Orendurff et al. ⁸²	8	Non-vascular	TF	48.5 ± 10.2	7/1	1.31 ± 0.12	C-leg <i>Mauch SNS knee</i>
Rosenblatt et al. ⁸³	8	Non-vascular	TT	53.3 ± 13.0	7/1	1.23 ± 0.29	Vacuum Assisted Socket System <i>Non- Vacuum Assisted Socket System</i>
Schmalz et al. ⁸⁴	8	Non-vascular	TT	44 ± 17	Unknown	1.33 ± 0.08	Flex-Foot <i>Otto Bock foot</i>
	6	Non-vascular	TF	33 ± 6		1.11 ± 0.03	Optimal alignment (3R80)
Seymour et al. ⁸⁵	13	Non-vascular	TF	46 ± 13	11/2	0.82 ± 0.25	C-leg <i>Non-microprocessor control knee</i>
Smith & Martin ⁸⁶	6	Non-vascular	TT	47 ± 16	5/1	1.18 ± 0.12	Genesis II, College Park or FlexFoot
Starholm et al. ⁸⁷	8	Non-vascular	TF	46.63 ± 13.19	4/4	0.82 ± 0.21	C-leg or hydraulic knee joint and ICS socket or quadrilateral socket
Tekin et al. ⁸⁸	10	Non-vascular	TT	27.7 ± 5.31	10/0	0.83	-

Torburn et al. ⁸⁹	9	Non-vascular	TT	50.6 ± 15.6	9/0	1.37 ± 0.28	Flex-Foot <i>SACH/ Carbon Copy II/ Seattle Lite/ Quantum</i>
	7	Vascular	TT	62 ± 8.3	7/0	1.03 ± 0.15	Flex-Foot
Traballesi et al. ⁹⁰	7	Non-vascular	TF	33.9 ± 9.4	6/1	1.10 ± 0.08	Ischial Containment Socket <i>Marlo Anatomical Socket</i>
Traballesi et al. ²⁷	8	Vascular	TT	56 ± 17	6/2	0.66 ± 0.26	Patellar tendon bearing hard socket ad energy storing foot
	16	Vascular	TF	61 ± 11	11/5	0.45 ± 0.17	Quad socket, polycentric knee joint and SACH foot

APPENDIX 3 – Overview study protocols**Analysis 1**

Study	Speed	Ground	Protocol	VO₂ analysis
Carse et al. ⁴⁷	PWS	Overground; 12 m walkway	6 minutes walking, mean over last minute	Open circuit spirometry, breath by breath
Chin et al. ⁴⁸	Fixed	Track with circumference 100 m	5 minutes walking, mean over last 2 minutes	Open circuit spirometry, breath by breath
Esposito et al. ¹⁸	PWS	Treadmill	5 minutes walking, mean over last 2 minutes	Open circuit spirometry, breath by breath
Gailey et al. ⁴⁹	Fixed	Treadmill	9 minutes walking, mean over last 3 minutes	Open circuit spirometry
Gailey et al. ⁵⁰	Fixed	Track with length 36 m	Measurement during last 3 minutes	Open circuit spirometry
Ganguli et al. ⁵¹	Fixed	Track with length 1 km	20 minutes walking	Douglas bag gas analysis
Gardinier et al. ⁵²	PWS	Track with length 8 m	8 minutes walking, 150 s used for analysis	Open circuit spirometry, breath by breath
Genin et al. ²⁵	Fixed	Outdoor track with length 41 m	Walking as long as needed maintain steady state for 3 minutes	Open circuit spirometry, breath by breath
Gitter et al. ⁵³	PWS	Overground	-	Douglas bag gas analysis
Gjovaag et al. ⁵⁴	PWS	Treadmill	3 minutes walking, mean over last 30 seconds	Open circuit spirometry, breath by breath
Gjovaag et al. ⁵⁵	PWS	Track with length 40 m	7 minutes walking, mean over last 2 minutes	Open circuit spirometry, breath by breath

Houdijk et al. ⁹	PWS	Treadmill	5 minutes walking, mean over last 2 minutes	Open circuit spirometry, breath by breath
Hsu et al. ⁹¹	Fixed	Treadmill	4 minutes walking, mean over last minute	Open circuit spirometry, breath by breath
Hunter et al. ⁵⁷	Fixed	Treadmill	5 minutes walking, mean over last minute	Open circuit spirometry
IJmker et al. ⁵⁸	PWS	Treadmill	5 minutes walking, mean over last 2 minutes	Open circuit spirometry, breath by breath
Jarvis et al. ⁵⁹	PWS	Track with length 10 m	5 minutes walking, mean over last minute	Open circuit spirometry
Mengelkoch et al. ²¹	PWS	Treadmill	Mean over last 20 seconds	Open circuit spirometry, breath by breath
Mengelkoch et al. ⁶⁰	PWS	Treadmill	Mean over last 20 seconds	Open circuit spirometry, breath by breath
Paysant et al. ²³	PWS	Overground	10 minutes walking, mean over last 2 minutes	Open circuit spirometry
Russell-Esposito ¹⁹	PWS	Treadmill	5 minutes walking, mean over last 2 minutes	Open circuit spirometry, breath by breath
Russell-Esposito ⁶¹	PWS	Treadmill	8 minutes walking, mean over last 2 minutes	Open circuit spirometry, breath by breath
Russell-Esposito ⁶²	PWS	Level ground	6 minutes walking, mean over last 2 minutes	Open circuit spirometry, breath by breath
Starholm et al. ²⁴	PWS	Track with length 40 m	7 minutes walking, mean over last 2 minutes	Open circuit spirometry, breath by breath
Waters et al. ⁶	PWS	Track with circumference 60.5 m	5 minutes walking, mean over last 2 minutes	Douglas bag analysis

Wezenberg et al. ²⁶	PWS	Treadmill	4 minutes walking, in order to reach steady-state	Open circuit spirometry, breath by breath
Analysis 2				
Askew et al. ⁶³	Fixed	Treadmill	7 minutes walking, mean over last 2 minutes	Open circuit spirometry
Barth et al. ⁶⁴	PWS	Treadmill	10 minutes walking, mean over last 3 minutes	Open circuit spirometry, breath by breath
Bell et al. ⁶⁵	PWS	Track, length 65 m	10 minutes walking, mean over last 2 minutes	Open circuit spirometry, breath by breath
Bellmann et al. ⁶⁶	PWS	Level ground	5 minutes walking, mean over last minute	Open circuit spirometry, breath by breath
Buckley et al. ⁶⁷	PWS	Treadmill	6 minutes walking, mean over last 3 minutes	Open circuit spirometry
Buckley et al. ⁶⁸	PWS	Treadmill	6 minutes walking, mean over 30 second intervals	Open circuit spirometry, breath by breath
Cao et al. ⁶⁹	Fixed	Treadmill	3 minutes walking	Open circuit spirometry, breath by breath
Casillas et al. ⁷⁰	PWS	Flat indoor surface	8 minutes walking, mean over last 2 minutes	Douglas bag
Darter & Wilken ⁷¹	Fixed	Treadmill	5 minutes walking, mean over last 2 minutes	Open circuit spirometry, breath by breath
Darter et al. ⁷²	Fixed	Treadmill	4 minutes walking, mean over last minute	Open circuit spirometry, breath by breath
Detrembleur et al. ⁷³	PWS	Treadmill	Walk 2 minutes after steady-state was reached	Open circuit spirometry, breath by breath

Goktepe et al. ⁷⁴	Fixed	Treadmill	5 minutes walking, mean over last 2 minutes	Open circuit spirometry, breath by breath
Grabowski et al. ⁷⁵	Fixed	Treadmill	9 minutes walking, mean over last 4-6 minutes	Open circuit spirometry
Graham et al. ⁷⁶	Fixed	Treadmill	2 minutes walking, mean over last 20 seconds	Open circuit spirometry, breath by breath
Houdijk et al. ¹⁶	PWS	Overground	4 minutes walking, mean over last 2 minutes	Open circuit, spirometry, breath by breath
Hsu et al. ⁷⁷	PWS	Treadmill	4 minutes walking, mean over last minute	Open circuit spirometry, breath by breath
Kirker et al. ⁷⁸	PWS	Treadmill	4 minutes walking	Closed system
Lin-Chan et al. ⁷⁹	Fixed	Treadmill	4 minutes walking, mean over last minute	Open circuit spirometry, breath by breath
Macfarlane et al. ⁹²	Fixed	Overground	-	Open circuit spirometry
McDonald et al. ⁸¹	PWS	Treadmill	6 minutes walking, mean over last 3 minutes	Open circuit spirometry, breath by breath
Orendurff et al. ⁸²	PWS	Overground	Walking until 2 minutes of steady-state were reached	Open circuit spirometry, breath by breath
Rosenblatt et al. ⁹³	PWS	Overground	6 minutes walking, mean over last 2 minutes	Open circuit spirometry, breath by breath
Schmalz et al. ⁸⁴	PWS	Treadmill	5 minutes walking, mean over last 30 seconds	Open circuit spirometry, breath by breath
Seymour et al. ⁸⁵	PWS	Treadmill	3 minutes walking, mean over last 30 seconds	Open circuit spirometry, breath by breath

Smith & Martin ⁸⁶	PWS	Treadmill	10 minutes walking, mean over last 2 minutes	Open circuit spirometry
Starholm et al. ⁸⁷	PWS	Treadmill	10 minutes walking, mean over last 5 minutes	Open circuit spirometry, breath by breath
Tekin et al. ⁸⁸	Fixed	Treadmill	5 minutes walking, mean over last 2 minutes	Open circuit spirometry, breath by breath
Torburn et al. ⁸⁹	PWS	Track, length 60.5 m	5 to 20 minutes walking, mean over minutes 4 to 5, 9 to 10, 14 to 15 and 19 to 20	Open circuit spirometry, breath by breath
Traballesi et al. ⁹⁰	PWS	Track, length 61 m	7 minutes walking, mean over last 2 minutes	Open circuit spirometry, breath by breath
Traballesi et al. ²⁷	PWS	Track, length 61 m	7 minutes walking, mean over last 2 minutes	Open circuit spirometry, breath by breath

APPENDIX 4 – Modified Newcastle-Ottawa Scale

Selection

- 1) Representativeness of patient group (1)
 - *One star was awarded when in- and exclusion criteria were described.*
- 2) Representativeness of patient group (2)
 - *One star was awarded when patient characteristics were described (i.e. age, sex, level of amputation, cause of amputation, type of prosthesis, time since amputation).*
- 3) Selection of patient group
 - *Studies that provided a detailed description of the recruitment of patients were awarded a star (where were patients included, how many patients were screened, and how many of them eventually participated).*
- 4) Selection of control group
 - *Studies that selected control subjects from the same community as people after amputation were awarded a star.*

Comparability

- 5) Comparability of groups (1)
 - *One star was awarded when possible confounders were reported. At least three of the following confounders should be obtainable: age, sex, physical fitness (e.g. BMI, hours of physical activity per week), preferred walking speed.*
- 6) Comparability of groups (2)
 - *One star was awarded when groups were matched with regard to possible confounders or if confounders were statistically corrected for. At least 1 of the 2 following should be taken into account: age and sex.*
- 7) Comparability of groups (3)
 - *One star was awarded when groups were matched with regard to physical fitness or physical activity level.*

Outcome

- 8) Assessment of outcome (1)
 - *One star was awarded if the applied protocol was clearly described in terms of instructions, duration and environment.*
- 9) Assessment of outcome (2)
 - *One star was awarded if the measurement methods were clearly described in terms of the system that was used for measuring oxygen consumption.*
- 10) Assessment of outcome (3)
 - *One star was awarded if the data analysis was clearly described in terms of using steady-state values, averaging oxygen consumption and duration of the analysed period.*
- 11) Follow-up adequacy
 - *One star was awarded if $\leq 10\%$ of the subjects that were initially included dropped out of the study / were not included in the final analysis. If no information was provided on this specific topic this was indicated with a question mark.*

APPENDIX 5 – Risk of bias assessment

Analysis 1												
Study	1	2	3	4	5	6	7	8	9	10	11	NOS score
Carse ⁴⁷	*	*	*		*	*	*	*	*	*		9
Chin ⁴⁸	*	*				*		*	*	*	?	6
Esposito ¹⁸	*	*			*	*		*	*	*	?	7
Gailey ⁴⁹	*	*			*	*		*	*		?	6
Gailey ⁵⁰	*	*			*	*	*	*	*	*	?	8
Ganguli ⁵¹						*		*	*		?	3
Gardinier ⁵²	*	*	*		*	*		*	*	*	*	9
Genin ²⁵								*	*		?	2
Gitter ⁵³					*				*		?	2
Gjovaag ⁵⁴	*	*			*	*	*	*	*	*	?	8
Gjovaag ⁵⁵	*	*			*	*	*	*	*		?	7
Houdijk ⁹	*					*		*	*		?	4
Hsu ⁵⁶	*				*	*		*	*	*	?	6
Hunter ⁵⁷						*		*	*		?	3

IJmker ⁹⁴	*			*	*	*	*	*	*	*	8			
Jarvis ⁵⁹	*	*		*	*		*	*		?	6			
Mengelkoch ²¹	*	*	*	*	*	*		*		*	8			
Mengelkoch ⁶⁰	*	*	*	*	*	*		*		*	8			
Paysant ²³	*	*		*	*	*	*	*		?	7			
Russell-Esposito ⁶²	*	*			*		*	*	*	?	6			
Russell-Esposito ⁶¹	*	*			*		*	*	*	?	6			
Russell-Esposito ¹⁹	*		*	*	*	*	*	*	*	*	9			
Starholm ²⁴	*	*	*	*	*	*	*	*	*	?	9			
Waters ⁶	*						*	*	*	?	4			
Wezenberg ²⁶	*			*	*	*	*	*	*	*	8			
Analysis 2														
Askew ⁶³		*					*	*	*		?	4		
Barth ⁶⁴	*	*					*		*		*		?	4
Bell ⁶⁵	*						*		*	*	*		?	4
Bellmann ⁶⁶	*	*					*		*	*	*	*	*	6
Buckley ⁶⁷		*					*		*	*	*	*	*	5
Buckley ⁶⁸									*	*		*		3

Cao ⁶⁹	*			*	*		?	3
Casillas ⁷⁰	*	*		*	*		?	4
Darter & Wilken ⁷¹	*	*		*	*	*		5
Darter & Wilken ⁷²	*	*		*	*	*		5
Detrembleur ⁷³	*	*			*	*		4
Goktepe ⁷⁴	*	*		*	*	*	?	5
Grabowski ⁷⁵		*		*	*	*	?	4
Graham ⁷⁶	*			*	*	*	*	5
Houdijk ¹⁶	*			*	*	*	?	4
Hsu ⁷⁷	*	*		*	*	*	*	6
Kirker ⁷⁸	*	*		*	*		*	5
Lin-Chan ⁷⁹	*	*		*	*	*	?	5
Macfarlane ⁸⁰	*	*		*	*		*	5
McDonald ⁸¹	*	*		*	*	*		5
Orendurff ⁸²				*	*			2
Rosenblatt ⁸³	*		*	*	*	*	*	6
Schmalz ⁸⁴	*			*	*	*	?	4
Seymour ⁸⁵	*	*		*	*	*		5

Smith & Martin ⁸⁶	*	*		*	*	*	?	5	
Starholm ⁸⁷	*	*	*		*	*	*	?	6
Tekin ⁸⁸	*				*	*	*	?	4
Torburn ⁸⁹	*				*	*	*		4
Traballesi ⁹⁰	*	*			*	*	*		5
Traballesi ²⁷	*				*	*	*	?	4

List of figures

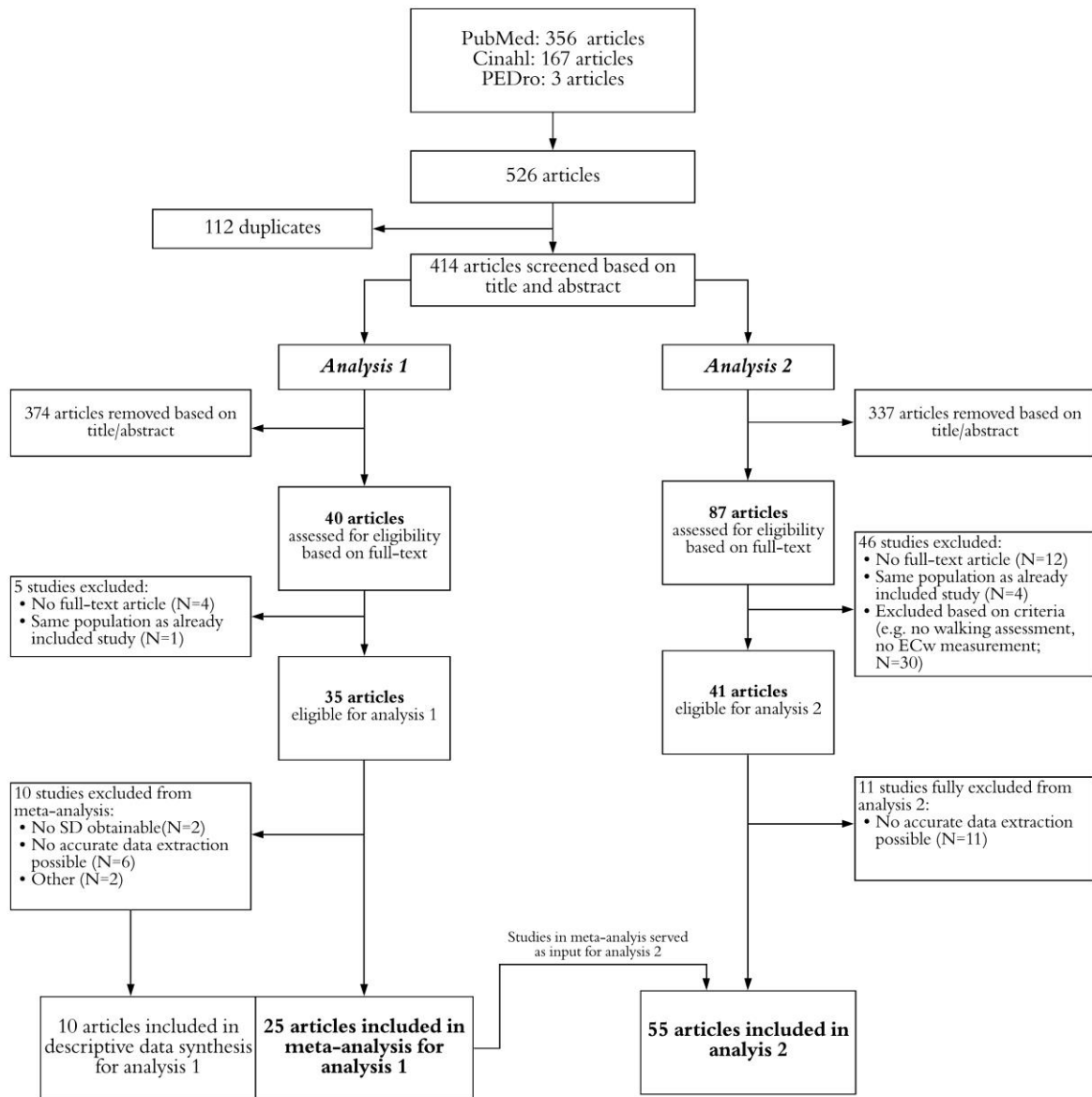


Figure 1. Flow-chart of inclusion of articles.

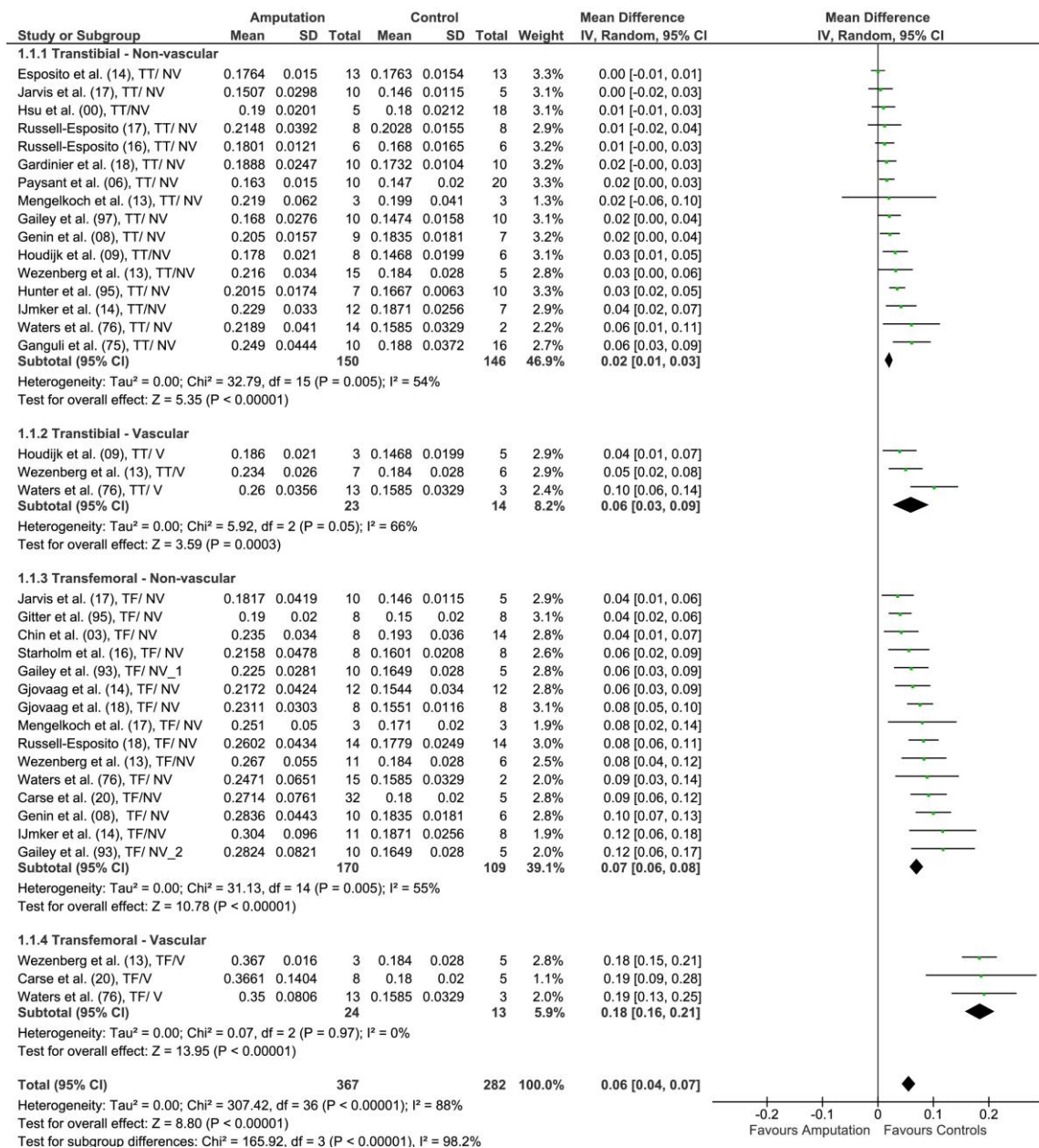


Figure 2. Pooled results of studies that investigated ECw in people with a lower limb amputation. TF/NV = transfemoral, non-vascular amputation; TF/V = transfemoral, vascular amputation; TT/NV = transtibial, non-vascular amputation; TT/V = transtibial, vascular amputation. NB1: Average preferred walking speed for each group was as follows; transtibial non-vascular: $1.20 \pm 0.51 \text{ m s}^{-1}$; transtibial vascular: $0.82 \pm 0.15 \text{ m s}^{-1}$; transfemoral non-vascular: $1.02 \pm 0.20 \text{ m s}^{-1}$; transfemoral vascular: $0.62 \pm 0.11 \text{ m s}^{-1}$. NB2: For two of the included studies,^{55, 59} standard deviation was obtained using Equation (2), as no other methods could be applied. However, this equation is typically recommend for studies with larger samples. To investigate whether using this equation influenced our results, we performed the meta-analysis also without these two studies, but this had minimal effect on the outcomes, and the main and subgroup remained unaffected.

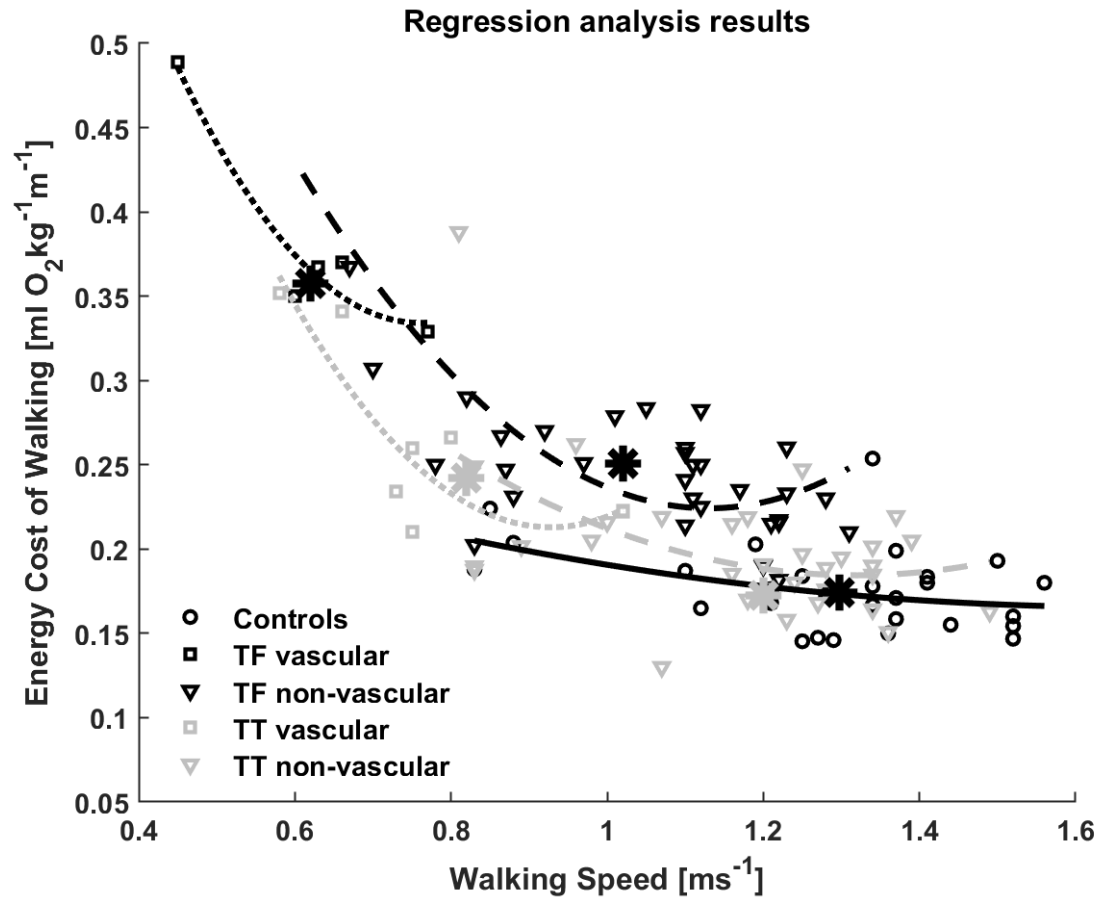


Figure 3. The effect of velocity on ECw. The average ECw and walking speed derived from analysis 1 is indicated with an asterisk (*) for each subgroup. CO = controls; TT = transtibial; TF = transfemoral. The values of the coefficients a , b and c represent the description of the second order polynomial function for each subgroup. CO: $a=0.06$, $b=-0.19$, $c=0.32$, $R^2 = 0.17$; TF vascular: $a=1.58$, $b=-2.40$, $c=1.24$, $R^2 = 0.93$; TF non-vascular: $a=0.73$, $b=-1.66$, $c=1.16$, $R^2 = 0.60$; TT vascular: $a=1.23$, $b=-2.28$, $c=1.27$, $R^2 = 0.75$; TT non-vascular: $a=0.27$, $b=-0.72$, $c=0.66$, $R^2 = 0.27$.

List of Tables

Table 1: overview of number of articles included in the different analyses by level and cause of amputation.

	Analysis 1 – influence of level and cause of amputation on ECw	Analysis 2 – influence of walking speed on ECw
	<i>(25 articles, describing 37 subgroups)</i>	<i>(55 articles, describing 78 subgroups)</i>
Transfemoral – Vascular	3	5
Transfemoral – Non-Vascular	15	32
Transtibial – Vascular	3	9
Transtibial – Non-Vascular	16	32

NB: Please keep in mind that the number of articles and subgroups shown for *analysis 2* is equal to the sum of the articles in *analysis 1* and the additionally included articles in *analysis 2*.

Table 2. Overview of pairwise comparisons of ECw between different subgroups.

	<i>Transfemoral – Vascular</i>	<i>Transfemoral – Non-Vascular</i>	<i>Transtibial – Vascular</i>	<i>Transtibial – Non-Vascular</i>
<i>Transfemoral – Vascular</i>		$\chi^2(1)=60.05$ $p < 0.00001^*$ $I^2= 98.3\%$	$\chi^2(1)=33.78$ $p < 0.00001^*$ $I^2= 97\%$	$\chi^2(1)=141.11$ $p < 0.00001^*$ $I^2= 99.3\%$
<i>Transfemoral – Non-Vascular</i>			$\chi^2(1)=0.30$ $p = 0.580$ $I^2= 0\%$	$\chi^2(1)=42.63$ $p < 0.00001^*$ $I^2= 97.7\%$
<i>Transtibial – Vascular</i>				$\chi^2(1)=5.28$ $p = 0.020^*$ $I^2= 81\%$
<i>Transtibial – Non-Vascular</i>				