Accurate Left Ventricle Segmentation and Ejection fraction estimation with Deep Learning-based Echocardiography

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Abstract

Heart failure with reduced ejection fraction is a rapidly growing public health issue with an estimated prevalence of over 37 million individuals globally. We proposed an efficient deep learning framework of automated echocardiography for predicting heart failure with reduced ejection fraction, which is most important for earlier diagnosis of heart function. The proposed deep learning framework sensibly overcame the echocardiography challenges which are domain expertise much needed for segmenting the left ventricular end-diastolic volume and end-systolic volume, high complexity in the identification of endocardial border and tiny labelled data. Due to advancements of artificial intelligence, we were able to address the challenges through a technique called data augmentation. three different deep learning models have been applied, the first model is UNet model, while the second model is Deeplab, and the third model is UNet model with backbone network for automated segmentation of left ventricle. The deep learning model has successfully segmented the left ventricle region on apical 4-chamber (A4C) views. The first model of UNet has mean IOU of 74.31%, and the second model of Deeplab has mean IOU of 79.53%. The proposed

model has achieved promising mean IOU of 89.1 % in segmentation and predicted ejection fraction with a correlation coefficient r^2 of 0.71. Results show that the contactless echocardiographic approach can quantitatively estimate left ventricular chamber size and ejection fraction in humans as well as estimate the dimensions of the left ventricle in systole and diastole.

Keywords: echocardiography, left ventricle, ejection fraction, deep learning, backbone

1. Introduction

A personalized and prospective approach to care is urgently needed to address heart failure, which is the leading cause of hospitalizations and deaths worldwide. Echocardiograms (Echo) are inviolable tests that use ultrasound to produce images of the heart [1-3]. The images allow doctors to assess the size, shape, and motion of the heart [4]. Medical images can be investigated more efficiently and accurately by deep learning algorithms, which are subsets of machine learning algorithms [5-13].

Echocardiography serves as a critical imaging technique for assessing cardiac structure and function in the diagnosis, management, and monitoring of cardiovascular diseases [14]. Accurate segmentation of cardiac structures from echocardiograms is crucial for quantitative analysis, visualization, and clinical decision-making. Furthermore, the estimation of ejection fraction (EF) from echocardiograms plays a pivotal role in evaluating cardiac performance and aiding in the diagnosis and prognosis of various cardiac conditions.

The EF is calculated by measuring the amount of blood that is pumped out of the left ventricle per beat. A normal EF varies between 55-70%, while an EF of less than 40% indicates reduced left ventricle outflow and is an important marker of heart failure. Cardiac diseases can be diagnosed and managed through echocardiography. Clinical decision-making requires precise and reliable echocardiographic assessment [15].

Perhaps the most significant indicator of cardiac function is the assessment of left ventricular EF, which is the ratio variation in the left ventricular end-systolic and enddiastolic volumes. This metric indicates individuals who are eligible for life-prolonging treatments [15, 16]. An overview of the need for automated echocardiography diagnosis is presented, along with a discussion of the application of artificial intelligence (AI) to echocardiography and its prospects.

The application of AI into everyday clinical practice and its potential to become an 25 invaluable tool for healthcare professionals who deal with cardiovascular diseases is 26 presented [17]. Myocardial reliable diagnosis is dependent on two-dimensional 27 echocardiography image quality. Images produced through scattering centres do not 28 have crisp edges like natural images. Therefore, to produce clear images, algorithms 29 are used to detect and suppress the scattering centres. This helps reduce the noise 30 and improves the image quality, aiding in the accurate diagnosis of myocardial 31 conditions. 32

Echocardiogram segmentation entails the precise delineation of specific cardiac structures such as the left ventricle (LV), right ventricle (RV), atria, and heart valves [18, 19]. Accurate segmentation enables the quantification of essential parameters including chamber volumes, wall thickness, and valve dimensions, facilitating a comprehensive assessment of cardiac function. Moreover, segmentation techniques contribute to the identification and tracking of pathological abnormalities such as ventricular hypertrophy, valvular disorders, and myocardial infarctions.

U-Net is a popularly used architecture for medical image segmentation because it 40 could localize and produce the underlying pattern [20]. It is a convolutional neural 41 network made up of a bottleneck layer connecting the encoder and the decoder. High-42 level features are extracted from the input image by the encoder, and the decoder 43 uses these features to reconstruct the segmented image [21]. In several medical 44 imaging tasks, including the segmentation of brain tumours [22] and vessels in the 45 retina [23, 24], U-Net has been demonstrated to perform better than other 46 47 segmentation methods. Its success can be attributed to two things which are its capacity to extract local and global information from the input image, as well as its 48 49 effective use of training data via data augmentation [25] methods. U-Net has also been modified for use in various other fields, including satellite imagery [26, 27]. 50

Moreover, deep learning has the potential to assist beginners in rapidly acquiring proficiency in quality diagnostic imaging, thereby enhancing both inter- and intraobserver consistency [28, 29]. Neural network models are trained by feeding them a sizable collection of labelled echocardiography data, where segmentation masks are established for different cardiac components as the Left Ventricle, Right Ventricle, and Mitral valve [30]. Following training, the model may be used to autonomously isolate

57 different heart components in new echocardiography pictures [31]. These models 58 when trained with large dataset and fine-tuned can also be used for real-time 59 segmentation during an echocardiogram procedure which can be useful for the 60 physicians [32].

It is important to recognize that deep learning has gained significant traction within 61 medical imaging with particular focus on its applications towards echocardiography. 62 Subsequently continual advancement in the area has introduced new techniques, 63 models, and insights [33]. One notable model advancement is the success of 64 Convolutional Neural Networks (CNNs) in autonomously segmenting echocardiogram 65 images [34]. Further upscaling of these CNN models can be employed through fine 66 tuning specific dataset/ applications for better performance and flexibility. Alternatively, 67 68 data augmentation techniques [35-37] can also expand a models' training set and enhance adaptability. 69

A comparison is then made between the model's segmentation results and the ground 70 71 truth labels, using metric such as the mean Intersection over Union (IoU). These measures give a quantitative assessment of the model's performance and provide a 72 way to compare the results with other models or different methods. It is important to 73 notice that the results of UNET on Echo segmentation vary based on the quality of 74 images, and the dataset used for training and testing, it also needs to be reviewed by 75 an expert cardiologist to have final verdict. Echocardiogram image segmentation 76 77 involves the process of identifying and separating different structures of the heart in an echocardiogram image. The segmentation results can then be used to obtain 78 79 quantitative measures of the heart's function, such as the left ventricular ejection fraction (LVEF), which is an indicator of heart health. 80

In recent years, there have been several variations of the U-Net architecture that 81 incorporate backbone [38] networks. The backbone, an essential component within 82 the UNet architecture, stands as a cornerstone for achieving accurate and robust 83 medical image segmentation. Revered for its ability to capture both local intricacies 84 85 and global contextual information, the U-Net owes much of its prowess to this intricate network. Acting as a formidable feature extraction apparatus, the backbone serves to 86 extract high-level features from input images, allowing the U-Net to acquire a deep 87 understanding of the data and perform precise segmentation with finesse. At its core, 88

the backbone of the U-Net embodies a pre-trained convolutional neural network (CNN)
model, seamlessly integrated into the U-Net structure.

The selection of the backbone network warrants utmost consideration, as it determines 91 the U-Net's capacity to discern meaningful and discriminative features. Among the 92 venerated choices for the backbone lie networks such as VGG [39], ResNet [40], 93 DenseNet [41], and EfficientNet [42], esteemed for their exemplary performance in 94 various computer vision domains. These backbone networks are pre-trained 95 96 convolutional neural networks that are used to extract features from the input image before feeding it to the U-Net model. The use of backbone networks has been shown 97 98 to improve the performance of the U-Net architecture, especially when the size of the training dataset is limited. Here are some popular backbone networks that have been 99 100 used with the U-Net architecture:

101 ResNet: ResNet is a deep residual neural network that has been used as a backbone 102 network for the U-Net architecture. It consists of several layers of residual blocks that 103 allow the network to learn more complex features, and it has been pre-trained on the 104 ImageNet dataset. Densenet: DenseNet's dense connectivity and feature reuse 105 mechanism make it a powerful deep learning architecture. It tackles the challenges of 106 information flow and promotes effective feature utilization, leading to improved 107 accuracy and better utilization of network parameters.

108 Deeplab: DeepLab framework addresses the challenges of dense pixel-level labelling 109 by leveraging the power of deep convolutional networks. It utilizes a modified version of the popular VGG-16 or ResNet network as the backbone for feature extraction. 110 These networks are pre-trained on large-scale image classification datasets, enabling 111 them to capture rich and transferable features. Therefore, the purpose of this study is 112 as follows. By using a pre-trained backbone network as the input to the U-Net 113 architecture, the network can leverage the powerful feature extraction capabilities of 114 the backbone network, while still maintaining the ability to perform precise localization 115 through the symmetric expanding path of the U-Net architecture. 116

117 **2. Methods**

In this study, we propose deep learning-based method for LV segmentation and ejection fraction estimation. Our method is based on a U-Net architecture, which is a convolutional neural network that has been shown to be effective for medical image

segmentation. The left ventricle segmentation workflow starts with dataset acquisition of echocardiogram videos obtained from the patients suspected of having heart failure and normal patients. Furthermore, the data pre-processing is followed by extracting the frames and de-identification of confidential information in the frames. The workflow for echocardiography segmentation and Ejection Fraction (EF) estimation can be summarized as follows:

127 2.1 Dataset

The dataset is produced and developed inhouse for this study. The inhouse dataset consists of echo videos in the form of apical four-chamber view. The data acquisitions were done from the National Taiwan University Hospital, Hsinchu branch, Taiwan. The study population includes both male and female with normal and reduced ejection fraction clinically indicated standard echocardiography.

To access the echocardiography data for research purposes, the study obtained 133 ethical approval from the Research Ethics Committee at National Taiwan University, 134 Hsin-chu Branch. The approval was granted under reference number 110-069-E, 135 ensuring compliance with ethical guidelines, and safeguarding the rights and privacy 136 of the individuals involved in the data collection. The echocardiography examinations 137 138 were conducted exclusively using state-of-the-art Philips ultrasound machines, ensuring standardized imaging protocols throughout the study. The acquired images 139 140 possessed a consistent frame resolution of 800 × 600 pixels, enabling a clear and detailed visualization of cardiac structures. 141

In consideration of the inherent physiological diversity among patients, both the frame rate (FR) and heart rate (HR) exhibited variations across the dataset. The frame rate, representing the frequency at which consecutive frames were captured, ranged between 25 and 66 Hz, accommodating diverse cardiac motion dynamics encountered during acquisition. Similarly, the heart rate, denoting the number of beats per minute, spanned a range of 60 to 150 beats per minute, reflecting the unique physiological profiles of the subjects.

By accounting for these fluctuations in frame rate and heart rate, the study acknowledged and accommodated the inherent variability in cardiac activity across the diverse patient population. This comprehensive approach ensured that the acquired data encapsulated a broad spectrum of cardiac dynamics, enhancing the

applicability and robustness of the subsequent analysis and findings. The dataset was
partitioned such that 80% of the data was allocated for training purposes, 10% for
validation to fine-tune the model's performance, and the remaining 10% for rigorous
testing to evaluate its generalization capability as shown in Table 1.



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In Figure 1, the distribution of ejection fraction (EF) is depicted for a cohort of 1000 patients. In accordance with clinical guidelines, when the Left ventricular ejection fraction (LVEF) falls below 40%, it is classified as reduced EF, indicating compromised cardiac function. Left Ventricular Ejection Fraction falling within the range of 40-49% is considered borderline, indicating a potential deviation from normal cardiac function. On the other hand, if the LVEF surpasses 50%, it is classified as normal, signifying a healthy level of ventricular contraction.



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Figure 1 Ejection fraction Distribution for 1000 patients

168 It is noteworthy to mention that the distribution of EF values suggests a class 169 imbalance within the data as shown in Figure 1. This implies that the number of samples representing different EF ranges may vary significantly, potentially leading to
 challenges in model training and evaluation. Addressing this class imbalance is crucial
 to ensure fair representation and accurate performance assessment of the models
 developed for EF estimation.

174 2.2 Data annotation

All Apical 4 chamber (A4C) view frames were extracted from the Digital Imaging and 175 Communications in Medicine files and converted into images, which were cropped and 176 resized to 128 × 128 pixels. Each pixel was then normalized between 0 and 1 for 177 neural network training and prediction. In the first step, we have extracted the frames 178 from clips in 50 frames per second and then selected the key frames such as end 179 systolic (ES) and end diastolic (ED) as shown in the Figure 2, with the help of 180 emergency room experts from National Taiwan University Hospital, Hsinchu branch. 181 The data split into different batches and provided to the experts for key frame selection 182 and data annotation of the left ventricle. 183



Figure 2 Data Annotation. (a) The frames are extracted from the echocardiogram video. (b)
Domain experts select the key frames (ED and ES). (c) The frames are labelled to produce
qround truth

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189 2.3 Data quality assessment

One of the biggest challenges we face when trying to scale up deep learning is the need for large and high-quality annotations that describe the content of echocardiograph images. Semantic annotations involve labelling images with detailed descriptions of what's in them, like identifying objects, regions, or specific characteristics. The need for massive and clean collections of semantic annotations is a bottleneck for a few reasons: training Data, models need a lot of labelled training data to learn patterns and make accurate predictions. Having access to large, annotated datasets directly affects how well these algorithms perform and how well they can handle different scenarios. Ensuring the quality and accuracy of semantic annotations is crucial for training reliable models. To achieve clean collections of annotations, we must be careful to minimize errors, inconsistencies, or biases in the labelling process.

This involves implementing thorough quality control measures and having humans supervise the process, which adds complexity and more time. It's important to annotate images with diverse and comprehensive semantic information to build robust and inclusive machine learning models. This means we need annotations from various domains, perspectives, and cultural contexts. Obtaining a massive and diverse collection of annotations presents additional challenges in terms of data collection, collaboration, and management.

Generating high-quality semantic annotations often requires domain expertise and 209 skilled annotators who have a deep understanding of the task at hand. It can be 210 expensive to acquire and retain such expertise, which can become a bottleneck when 211 scaling up the learning process. To address these challenges, we need to develop 212 more efficient annotation methodologies, improve automation techniques, and 213 advance our data collection practices. Additionally, exploring alternative approaches 214 like weakly supervised learning or active learning can help reduce our dependence on 215 fully annotated datasets, which can help alleviate the bottleneck to some extent. 216

217 Figure 3 Illustrates the assessment of image quality using REDcap [43,44] electronic data capture tools hosted at National Taiwan University Hospital, Hsinchu branch, 218 Taiwan, used for performing the digital survey with a team of five novice volunteers. 219 The volunteers who are participating in the survey are provided with a short training 220 221 course of assessing the quality of frames, with constraints such as clear apical four chamber, sharp LV borders, good contrast, and the overall quality for the frames. 222 223 Based on the quality of frames, the volunteers will provide the rating for the frames on a scale of 1 to 10. A rating of 1-4 is considered poor quality, and a rating of 5-7 is 224 considered good quality. A rating of 8-10 indicates good image quality. 225

The quality of the 2D cross-sectional echo images is variable due to dependence on the experience level of the echo operators. Furthermore, the ultrasound quality may worsen with age, disease, and obesity, which coincidentally are correlated with heart disease risk. Direct cine-based EF estimation in echo is a challenging problem. Ultrasound images are inherently noisy and yield blurry chamber boundaries, making LV size changes difficult to quantify.





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Figure 3 Image Quality Assessment survey for a team of novice using Redcap.

Cardiac anatomy and function are complex and variable, especially in the apical views.
The complexity is compounded by variations in the appearance of the imaged heart in
the presence of pathology. Echo images only capture 2D cross-sectional views of the
heart, which may be foreshortened. LV foreshortening may inevitably lead to incorrect
measurements, even if the image analysis task is accurate.

240 2.4 Model

Our deep neural network architecture was designed in python[45] using the TensorFlow [46] and Keras [47] frameworks. Our model consists of convolutional layers with activation functions. Our model consisted of a succession of modest 3 × 3 convolutional filters connected with max-pooling layers spread across 2 × 2 windows. To counteract overfitting [48], dropout was used in training for both the convolutional and fully connected layers.

UNet utilizes an encoder-decoder structure with skip connections for image 247 segmentation, while ResNet34 employs residual blocks and skip connections to 248 enable training of very deep networks. UNet focuses on capturing hierarchical features 249 and recovering spatial information, while ResNet34 excels at handling deep networks 250 and learning residual mappings. The combination of these two architectures in the 251 UNet+ResNet34 model allows for efficient feature extraction, depth, and skip 252 connections, leading to improved performance in left ventricle segmentation task. In 253 our Model, the ResNet34 encoder is used to extract features from the input image, 254 255 and the U-Net decoder is used to reconstruct the output image.

256 2.5 Ejection fraction estimation

In semantic segmentation, the model will segment the area of left ventricle to estimate the ejection fraction using the equation as mentioned in Equation 1. The estimate of ejection fraction is based on the segmentation of echocardiograms' key frames. Based upon the ejection fraction, the heart function is classified. If the EF is between 50% to 70%, heart function is normal. Whereas the EF is between 41% to 49%, heart function is borderline. Reduced EF leads to heart failure if it is below 40%.

Left ventricular ejection fraction (LVEF) is one of the most reported measures of left ventricular (LV) systolic function. It is the ratio of blood ejected during systole (stroke volume) to blood in the ventricle at the end of diastole (end-diastolic volume). If the LV end-diastolic volume (EDV) and end-systolic volume (ESV) are segmented or annotated as shown in the Figures 4(a) and 4(b), LVEF can be determined using Equation 1:



$$LVEF = \frac{(EDV - ESV)}{EDV} \times 100$$
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Figure 5 Echocardiography segmentation and EF estimation workflow. (a) Echocardiography
videos are converted to frames and the key frames, End-Diastolic (ED) and End-Systolic (ES).
(b) The frames are rated by the volunteers according to the quality of the images. (c) After the
pre-processing step, data was segmented and predicted. (d) Key frames are the used for
Ejection Fraction (EF) estimation.

- Finally, the whole procedure is summarised in Figure 5. Echocardiography videos are converted to frames, and the key frames at End-Diastolic (ED) and End-Systolic (ES) phases are identified by emergency room experts (i.e., medical doctors). These videos are processed to extract individual frames, and the frames at the ED and ES phases represent the maximum and minimum volumes of the heart, respectively as shown in Figure 5(a).
- Volunteers or experts meticulously rate the frames on a scale of 1 to 10, assessing the quality of the images with utmost precision as shown in Figure 5(b). If the rating is in the range between 1 to 4, it is considered noisy data and frames with poor quality can be excluded from further analysis or flagged for additional scrutiny. If the rating falls within the range of 5 to 7, it is deemed acceptable. When the rating falls within

the range of 8 to 10, it serves as an indication that the data is impeccably clean and boasts exceptional quality. This quality assessment step helps filter out frames that may be affected by artifacts, motion blur, or other factors that could potentially affect the accuracy of segmentation and EF estimation.

Pre-processing steps are applied to the selected frames to enhance their quality and facilitate accurate segmentation as shown in Figure 5(c). This involves image denoising, contrast adjustment. The pre-processing stage aims to remove noise and artifacts that could hinder the subsequent segmentation and EF estimation processes.

The pre-processed frames are then segmented to identify and delineate specific 297 298 structures of interest, the LV as shown in Figure 5(d). The segmentation step aims to precisely outline the boundaries of the structures, providing accurate spatial 299 300 information for subsequent analysis. Once the segmentation is complete, the key frames (ED and ES) are utilized for EF estimation. Ejection Fraction is a crucial metric 301 used to assess cardiac function and is calculated by comparing the volume of blood 302 pumped out of the LV during systole (ES phase) with the volume at maximum filling 303 during diastole (ED phase). The segmented regions corresponding to the LV are used 304 to measure the volumes, and the EF is calculated as the ratio of stroke volume to end-305 diastolic volume, often expressed as a percentage as shown in Figure 5 (d). 306

By following this workflow, echocardiography videos are processed into frames, key frames are identified, image quality is assessed, pre-processing is performed, segmentation is executed, and finally, EF estimation is conducted using the key frames. This workflow enables the assessment of cardiac function based on echocardiographic data, providing valuable insights for diagnosis, monitoring, and treatment planning in cardiovascular medicine.

313 3. Results

In this research, we show that left ventricle segmentation has been effectively clarified with a CNN-based U-Net architecture. IoU is a measure of how well two objects overlap [49]. The IoU formula requires an understanding of two key terms: True Positive (TP) and False Positive (FP). True Positive is when the model correctly predicts a pixel as being part of an object when it is part of the object. It is a False Positive when the model predicts that a pixel is part of an object when in fact it is part of the background. It is the ratio of the area of overlap between the two objects to the

area of their union according to the Equation 2. It is used in object detection and image
 segmentation tasks to measure the accuracy of the model's prediction.

$$IoU = TP / (TP + FP + FN)$$
(2)

Conventional methods cannot obtain such an IoU using clustering [50], threshold 323 segmentation [51], or machine learning algorithms [52]. The reason for this is that 324 regardless of which conventional method is used, there will always be a manual 325 selection process to determine colours, textures, or shapes. Despite this, different LV 326 borders in the dataset exhibit clearly distinct characteristics. However, by using an 327 image segmentation approach such as U-Net, this manual selection process can be 328 329 avoided, as U-Net is able to automatically identify and segment target objects from an 330 image.

This makes U-Net far more suitable for determining LV borders, as it can achieve a 331 much higher IoU score than conventional methods. Figure 6 illustrates (a) grey image 332 333 is input image to the model, (b) red region annotated by the experts (c) yellow region shows model could perform well on the left ventricle segmentation task. Left ventricle 334 boundary definition is crucial for treatment, but it is not easily accomplished during 335 segmentation of medical images, which is known as segmentation. Table 2 shows the 336 comparison of model performance, UNet has performed the automated LV 337 segmentation of echocardiogram 2D frames with mean IOU of 74.31%. 338

The proposed model, UNet with Resnet as backbone [38] network has outperformed 339 the Deeplab [53] and UNet base model with highest mean IoU of 89.12% on the LV 340 segmentation task for the 2D echo images. In comparison with the proposed model, 341 342 MaskRCNN [54], Echonet [55], and 3D-UNet [56] has higher mean IOU of 92.21%, 92%, and 93% respectively. According to Echonet [55], They have used massive 343 dataset of video recordings represent unique individuals because the dataset contains 344 videos recorded from 10,036 random echocardiography procedures performed 345 between the year of 2006 and 2018. 346

According to Table 2, to ensure data-centric models perform effectively, we require vast amounts of high-quality data. This means having datasets that are extensive and diverse, enabling the models to learn from a wide range of examples. However, it's not just about quantity; the data also needs to be meticulously cleaned, removing any

noise, errors, or inconsistencies. This ensures that the models can rely on accurateand trustworthy information during their training.

Expert annotation is another vital aspect of data-centric AI. Domain experts with deep knowledge in the relevant field provide precise labels or tags to the data. Their expertise ensures that the models learn from ground truth labels, enabling them to make accurate predictions and perform complex tasks.

Maintaining data quality is essential throughout the annotation process. Rigorous quality control measures are implemented to ensure the correctness and consistency of the annotations. Addressing biases and ensuring agreement among experts are critical steps in this process. Working together with domain experts plays a crucial role in developing comprehensive datasets. Their insights and understanding of the specific application area are essential for guiding the annotation process and capturing the domain's nuances.

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Table 2 Model Performance comparison

Base Model	Backbone	mean IoU (%)
UNet	-	74.31
Deeplab [53]	VGG16	79.53
MaskRCNN [54]	-	92.21
Echonet [55]	-	92.0
3D U-Net [56]	-	93.0
Proposed Model	Resnet50	89 12

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Figure 6 Models Segmentations samples. (a) Original image (b) Ground truth (c) Segmentation
Result

According to our approach for the help of emergency room experts from National 369 Taiwan University Hospital, Hsinchu branch, the data split into different batches and 370 provided to the experts for key frame selection and data annotation of the left ventricle. 371 Hence, we want to see what the differences between cardiovascular experts and 372 emergency room experts for labelling area then calculating LV of EF. Figure 7 shows 373 the comparison of correlation coefficients, (a) comparison of cardiovascular experts 374 and emergency room experts; (b) Comparison of cardiovascular experts and model 375 prediction; (c) comparison of model prediction and emergency room experts. The 376 377 correlation coefficient between the cardiovascular expert and emergency room experts is 0.9771, which exhibits the strong correlation coefficient and expertise of 378 domain knowledge. Therefore, we use emergency room experts to label then calculate 379 LV of EF is reasonable and acceptable. However, the correlation coefficient between 380 the cardiovascular expert and model prediction is 0.6904. Also, the correlation 381 coefficient between the model prediction and emergency room experts is 0.7122. This 382 shows the proposed model is needed to further improve the accurate estimates of LV 383 of EF based on the given input and output data in the near future. Although our 384 proposal model has been shown a little bit of less than accuracy in comparison with 385 386 previous research Echonet [55] model for using large database of 10,036 patients which are over 10 times of our patient data. 387







is needed to provide a more accurate assessment of the disease. This research aims
to examine the feasibility of using a combination of biomarkers to stratify heart failure
patients. The results of this study will provide valuable insight into the efficacy of using
multiple biomarkers for stratifying heart failure patients.

400 **4. Discussion**

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402 Our results suggest that deep learning is a promising technology for LV segmentation 403 and estimation of ejection fraction. Our method is more accurate and efficient than 404 manual segmentation, and it has the potential to improve the diagnosis and 405 management of heart disease. Deep learning has emerged as a powerful tool for 406 medical image analysis, and it has been shown to be particularly effective for 407 segmentation of the LV from the echocardiograms.

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Technically, deep learning models can learn to identify complex patterns of the LV 409 from the images, even in the presence of noise and other challenges. The use of deep 410 learning for LV segmentation has several potential benefits. First, it can automate the 411 segmentation process, saving time and improve the accuracy of measurements. 412 Second, deep learning models can be trained on large image datasets, which can 413 improve the accuracy of segmentation even in challenging cases. Third, deep learning 414 models can be used to segment images from different imaging modalities, which can 415 improve the precision of diagnosis and treatment planning. 416

Clinically, in the crowded emergency department, distinguishing potential patients with 417 418 moderate to severe heart failure and further to avoid impending cardiac collapse are difficult but crucial. Traditional physical examinations, such as heart sound 419 420 auscultation and heart border percussion, may not identify true emergency because of limited time in diagnosis and subjective judgment of the physicians. Automatic real-421 time detection of the left ventricle ejection fraction provided objective assessment of 422 the heart condition. Our proposed model, consistent with previous studies, assessed 423 the ejection fraction using the deep learning algorithm with excellent prediction 424 performance [58, 59]. However, some population and setting variations caused 425 different model prediction powers. In Liu's study in China, two open-source data sets 426 and one clinical data set were collected. The sample size of the mixed database was 427

large, but the heterogeneity thereby existed [58]. In Asch's study, which compared the 428 agreement of the reference ejection fraction (by experienced cardiologists) and the 429 prediction of the interclass correlation ranged from 0.86 to 0.95 with biases less than 430 2% [28]. In the study conducted in Norway, they indicated that the ejection fraction 431 was considerably affected by apical foreshortening using three-dimensional 432 ultrasound, and the mean absolute difference in their result was measured at 7.2%, 433 which are comparable with related studies [59]. The above results, whether 2D or 3D 434 echocardiography, implied that automatic deep learning-based prediction may work in 435 436 some circumstances without specialists.

Some limitations were noted in this study. First, deep learning models require large 437 datasets of labelled images to train, which can be expensive and time consuming to 438 439 collect. Second, deep learning models can be sensitive to changes in image quality, which can lead to errors in segmentation. Third, deep learning models can be 440 441 computationally expensive to train and deploy, which can limit their use in resourcelimited settings. Deep learning is a promising tool for segmenting the LV from 442 echocardiograms. It has the potential to automate the process of segmentation, 443 improve the accuracy of measurements, and make it possible to segment images from 444 different imaging modalities. 445

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In the coming future, in addition to the prediction of the left ventricle ejection fraction, 447 the prediction of the right heart function is drawing attention. The predictive 448 significance of RV has been well recognized [60]. It is not only the main determinant 449 450 of clinical symptoms and survival in patients with hypertension, but also has an independent predictive value for left heart disease. Approximately half of patients with 451 heart failure and reduced left ventricular output (LVEF) suffer from RV dysfunction, 452 which is associated with a double increase in the risk of side effects. The 453 implementation of right ventricular ejection fracture by the UNet model could be further 454 anticipated. 455

456 **5.** Conclusion

In summary, the present research demonstrated that the proposed model, which was
adapted for echocardiogram usually used in the clinical setting, enables automated
evaluation of LV of EF and, more specifically, detection of heart failure with accuracy

460 comparable to through imagery analysis by experienced imaging cardiac specialists.
461 Based on the results, the method shows clean data is essential for accurate and
462 reliable AI model training, while noisy data can introduce biases and inaccuracies. This
463 technique is likely to further improve for increasing more patient data so it can help
464 more health care providers to reliably conduct and analyse cardiac ultrasound
465 assessments.

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